### **3D workflows in maxillary prosthodontic rehabilitation of head and neck cancer patients**

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Author: Nathalie Vosselman Provided by thesis specialist Ridderprint, ridderprint.nl Printing: Ridderprint Layout and design: Jolanda Hiddink, persoonlijkproefschrift.nl

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The research presented in this thesis was performed and financed at the Department of Oral and Maxillofacial Surgery, University Medical Center Groningen, The Netherlands.

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### **3D workflows in maxillary prosthodontic rehabilitation of head and neck cancer patients**

**Proefschrift**

ter verkrijging van de graad van doctor aan de Rijksuniversiteit Groningen op gezag van de rector magnificus prof. dr. ir. J.M.A. Scherpen en volgens besluit van het College voor Promoties.

De openbare verdediging zal plaatsvinden op

vrijdag 12 juli 2024 om 16.15 uur

door

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geboren op 7 januari 1979

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## **CHAPTER**



#### **GENERAL INTRODUCTION**

Collaborative care of patients with head and neck cancer can be challenging particularly when it concerns diagnosis, treatment, and rehabilitation. Head and neck cancer doctors and dentists usually form a multidisciplinary team that care for the management of these cancers and develops individualized treatment plans for each patient. Oncological treatment options may include surgery, radiation therapy, chemotherapy or a combination of these treatments, depending on the stage, location and biological behaviour of the cancer, as well as the overall health of the patient<sup>1.</sup>

Tumours of the maxilla, while relatively uncommon, require multidisciplinary involvement due to their effects on the aesthetic, functional and psychological aspects of the patients involved<sup>2</sup>. Although sequelae of tumour resection are comparable in the majority of patients, details in the intermaxillary relations, facial morphology and functional capacity can vary significantly<sup>3</sup>.

Radiotherapy is a valuable treatment in the survival of head and neck cancer patients. When applied in the post operative setting, degeneration of oral functions after maxillectomy increase which can severely undermine the quality of life of the patients. The size and extent of the maxillary defect, patient factors, and comorbidities are decisive factors for the choice of surgical, prosthodontic, or combined rehabilitation after a partial maxillectomy. The use of classifications such as those by Brown<sup>4</sup> and Okay<sup>s</sup> are helpful tools to assist with surgical planning and decision-making in this complex area<sup>6</sup>. However, there is no clear or generally accepted recommendation to select the optimal method of obturation, reconstruction, and rehabilitation of the maxillary defects following tumour ablation<sup>7</sup>.

The head and neck oncology team must make patient-specific decisions regarding rehabilitation based on the extent and position of the maxillary defect. The overall objective in patients with oronasal communication is to follow a surgical or prosthodontic reconstruction strategy with the aim to restore impaired oral functions<sup>8</sup>. From that perspective, dental rehabilitation is an important consideration for achieving a good outcome<sup>9</sup> and a major step toward enhancing quality of life after controlling the disease.

#### **Obturator prostheses**

Historically, rehabilitation with an obturator prosthesis has been the most common approach to restore maxillary defects<sup>10</sup>. This classic way of prosthetic management in general involves a three staged approach involving a surgical, interim and definitive obturator prosthesis<sup>11</sup>. The surgical obturator is placed subsequently after tumour resection in the operating room and enables immediate rehabilitation of oral function. This is achieved by peroperative adapting a prosthesis to the new anatomic situation. Molding of a bulb extension secures obturation of the resection cavity. Fixation of the obturator in edentulous patients is generally ensured in the first weeks postoperative by screws in the palatal bone or zygomatic wiring, and when natural dentition remains after surgery clamps are used for retention. However, conventional obturator prostheses can have their drawbacks, mainly caused by lack of retention of the prosthesis<sup>12</sup>.

Especially in more extensive resections, there may be no or hardly any maxillary bone or teeth present to provide obturator support. Placement of endosseous implants in the remaining native bone of the maxilla can provide a platform for the fabrication of a retention bar that supports and retains the overlying obturator prosthesis. Unfortunately the amount of maxillary bone is often limited or insufficient for reliable implant placement due to alveolar bone resorption as well as due to the ablative surgery.

Given the average high age among head and neck oncology patients prolonged edentulism is frequently seen with severe atrophic maxilla bone and the presence of pneumatic sinuses. This disables utilisation of conventional implants to gain retention and support the obturator prostheses.



Classic design of a surgical, interim and definitive obturator prosthesis

#### **Zygomatic oncology implants**

The development of the "remote bone anchorage" concept paved the way for the use of zygomatic implants in the management of patients with maxillary tumour defects with the high-quality bone of the zygoma providing excellent anchorage for long implants cantilevered into the defect to provide prosthetic support and retention. With advancing techniques in this field, zygomatic implant design has evolved from the traditional implant design developed by Professor PI Branemark with roughened threads throughout the entire length to "oncology-zygomatic implants" with threads only at the implant apex to allow osseointegration in the zygomatic bone. These modified implants are more cleansable when exposed into maxillary defects. Although good outcomes are reported over the years, zygomatic implants are still not widely used in complex rehabilitation cases. Accurate placement of zygomatic implants, taking the preferred prosthodontic positioning into account, is considered difficult. In the absence of guiding anatomic references, it is challenging to place two zygomatic implants at the defect side because of the long drill path.

#### **Prosthodontic virtual surgical planning**

Advanced surgical techniques and the development of supportive care have contributed to improving outcomes and quality of life for patients with head and neck cancer. Among the emerging tools in Head and Neck cancer treatment is the use of threedimensional virtual surgical planning (3D VSP), which has shown significant potential in the creation of accurate and patient-specific virtual models of the maxillofacial region. This technology enables surgical teams to simulate and plan surgical procedures with greater accuracy, by providing insight into the extent of the tumour and facilitating the planning of the surgical approach. The integration of 3D VSP into the management of head and neck cancer has been shown to improve the predictability and accuracy of surgical outcomes, while reducing the duration of surgery time. High-complexity oncological conditions often require prosthodontic rehabilitation and implant support. Therefore preoperative planning process should not only consider surgical oncological treatment and reconstruction but also include the seamless integration of prosthodontic rehabilitation into the virtual plan. After tumour resection, complex anatomic alterations demand individualized prosthodontic rehabilitation approaches, requiring the expertise of the maxillofacial prosthodontist. Therefore, a synergy of various digital workflows regarding treatment and rehabilitation should enhance the best possible care for patients with head and neck cancer. The integration of digital prosthodontic workflows is a crucial step towards personalized and precise management of maxillary malignancies, emphasizing the importance of teamwork in enhancing patient care.

#### **AIM OF THE THESIS**

The general aim of this PhD thesis is to develop a digital prosthodontic pathway for complex rehabilitation of maxillary defects in Head and Neck cancer patients, with preplanning the surgical resection and reconstruction with 3D virtual surgical planning (3D VSP). The progress of three-dimensional technology, the pre-treatment insight in overall prognosis and possibilities of surgical rehabilitation has led to many new applications in head & neck oncology. However, few new 3D supported strategies have been developed for supporting the prosthodontic rehabilitation after maxillectomies. In contrary to the 3D workflow of the surgical treatment, the prosthodontic rehabilitation of Head and Neck cancer patients commonly is an analog workflow with minor digitalized steps. A combined and complete virtual maxillary resection, reconstruction, and prosthetic rehabilitation planning will enable the maxillofacial prosthodontist to follow a digital prosthodontic workflow and to make balanced decisions with the multidisciplinary Head and Neck Oncology team to shape and outline the prosthetic and dental rehabilitation in line with the surgical options. These topics will be addressed in this thesis.

The specific aims are:

- to systematically review the evolution of 3D techniques in prosthodontic rehabilitation of head and neck cancer patients. It offers a comprehensive overview of the prosthetic challenges in this patient group **(chapter 2).**
- to describe a complete 3D workflow for immediate implant-retained prosthetic rehabilitation following maxillectomy in cancer surgery. This workflow consist of a 3D Virtual Surgical Planning for tumour resection, zygomatic implant placement as well as for an implant-retained prosthetic-obturator to fit the planned outcome situation for immediate loading **(chapter 3)**.
- to assess the accuracy of the developed digital workflow for guided placement of zygomatic implants after maxillectomy and determine the usability of the procedure intraoperatively **(chapter 4).**
- to assess, in a prospective study, the implant survival and patient outcomes 1-3 year after guided placement of zygomatic implants in Head and Neck oncology patients. We visualize the tumour size and position and its direct impact on the radiation dose received by the zygomatic bone and implants **(chapter 5).**
- to combine the available 3D techniques of planning, designing and milling to produce a patient specific implant to support an obturator prosthesis. Our goal is to improve the severely impaired speech and swallowing, and a patient-specific subperiosteal implant (psSPI) is designed that matched the remnants of the zygoma complex **(chapter 6).**

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## **CHAPTER**

# 2.1

**Prosthodontic rehabilitation of head and neck cancer patients - challenges and new developments**

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*This chapter is an edited version of the manuscript: Prosthodontic rehabilitation of head and neck cancer patients - challenges and new developments.*

Oral Diseases 2021;27(1):64-72.

#### **ABSTRACT**

Head and neck cancer treatment can severely alter oral function and aesthetics, and reduce quality of life. The role of maxillofacial prosthodontists in multidisciplinary treatment of head and neck cancer patients is essential when it comes to oral rehabilitation and its planning. This role should preferably start on the day of first intake. Maxillofacial prosthodontists should be involved in the care pathway to shape and outline the prosthetic and dental rehabilitation in line with the reconstructive surgical options. With the progress of three-dimensional technology, the pre-treatment insight in overall prognosis and possibilities of surgical and/or prosthetic rehabilitation has tremendously increased. This increased insight has helped to improve quality of cancer care. This expert review addresses the involvement of maxillofacial prosthodontists in treatment planning, highlighting prosthodontic rehabilitation of head and neck cancer patients from start to finish.

#### **INTRODUCTION**

Head and neck cancer is the fifth most common cancer worldwide<sup>1</sup>. The course of the disease and its treatment have major effects on psychological well-being and functioning of the patients<sup>2</sup>. The treatment of head and neck cancers consists of different treatment modalities, typically being surgery, radiotherapy, chemotherapy or a combination of these modalities. Besides curing cancer, another important aim is to regain the oral function and aesthetics that got lost or altered due to the treatment.

Effects of primary oncology surgery can impede rehabilitation goals<sup>3</sup>. These effects include an altered oral anatomy, compromised soft tissue conditions like missing or scarred tissues and bulky flaps, altered muscle attachments and muscle balance, sensitivity disorders, loss of lip competence and trismus, loss of anatomical structures, loss of bony structures and/or teeth, and alterations in facial appearance. Regaining oral function and aesthetics is a challenge because of limitations in the restorative treatment options due to, e.g. poor support and lack of space for a prosthesis, impeded resilience of soft tissues, impaired tongue function, and loss of integrity and competence of the velopharyngeal complex<sup>4</sup>.

Posteriorly situated tumours, tumour size, adjuvant radiotherapy and extensive softpalate and tongue resections have been shown to be predictors for deterioration of oral functioning<sup>5-7.</sup> Studies that looked into the quality of life of head and neck cancer patients after completion of oncologic treatment reported that regaining oral function, including prosthetic rehabilitation, is of great importance<sup>8-10</sup>. Therefore, the oncological team is in need of specially trained, experienced dental professionals, preferably maxillofacial prosthodontists, to support the team with planning of the oral rehabilitating head and neck patients. This planning and treatment may include the use of osseo-integrated intra- and extra-oral implants to retain oral and/or facial prostheses .

As mentioned, to achieve rehabilitation goals, a close and open collaboration between ablative surgeons, reconstructive surgeons, radiation oncologists, maxillofacial prosthodontists and medical engineers is of utmost importance to move towards an optimal rehabilitation of the head and neck cancer patient. The purpose of this expert review is to emphasize the role of the maxillofacial prosthodontist in the treatment planning and oral rehabilitation of head and neck cancer patients as well as to discuss challenges and new developments in the prosthodontic rehabilitation of these patients.

#### **Pre-treatment screening**

Multidisciplinary first-day consultation intents to shorten time between diagnosis and treatment of oral cancer<sup>11</sup>. Maxillofacial prosthodontics should be included in the multidisciplinary first-day consultation. This first-day consultation aims to provide a preliminary plan stating the required diagnostic procedures and prosthetic involvement (Figure 1) so that treatment can start as soon as and as effective as possible. The involvement of the maxillofacial prosthodontist includes a pre-radiation dental screening, and a pre-treatment dental and oral rehabilitation screening $12$ . During this screening, all available information is gathered with regard to self-care, oral hygiene, dental situation, mouth opening, location of the suspected or confirmed tumour, presumed need for ablative surgery and/or radiotherapy, estimation of retention and bearing of a future (obturator, dental) prosthesis, and estimation of the pre-existent level of oral function<sup>13,14</sup>. This information is needed to design the best prosthetic treatment plan. This plan should be designed taking the patients' wishes, the tumour characteristics, extent of acquired resection for clean margins, possible types of reconstruction, need for (chemo)radiation, and dental and/or prosthetic possibilities into account.



**Figure 1.** Involvement of the maxillofacial prosthodontist in treatment planning and rehabilitation of head and neck cancer patients focused on ablative surgery. MD: Multidisciplinary, MFP: maxillofacial prosthodontics; Post-op: Post-operative, RT: radiotherapy; chemo: chemotherapy.

\*Preferably, implants are placed during ablative tumour surgery. When not feasible, implants can also be placed during follow-up. For details see Alberga et al. (2020).

#### **Pre-radiation dental screening**

In case radiotherapy might become involved, head and neck cancer patients in whom the oral cavity is within the radiation treatment portal are in need of a thorough dental examination. These patients have to complete any required dental treatment before the onset of radiotherapy<sup>15</sup>. Pre-radiation dental screening aims to locate and eliminate oral foci of infection, such as unrestorable caries, periodontal disease with pockets ≥6mm, periapical problems and (partially) impacted teeth $^{12}$ .

#### **Pre-treatment dental and oral rehabilitation screening**

Although at the first day consultation the extent of the final oncologic treatment plan is uncertain, at this stage the maxillofacial prosthodontists should already estimate whether patients are in need of a prosthetic rehabilitation simultaneously with reconstructive surgery or after completion of cancer therapy, and what the patients' desires are. Implementing the results of pre-treatment screening into the prosthetic workflow ensures that all information is gathered and all needed care is provided to design a patient specific prosthetic rehabilitation draft plan. In some cases, prosthetic retentive considerations are critical to achieve successful prosthetic rehabilitation. The size of the defect and number of critical remaining teeth that may serve as anchorage for conventional clasp supported removable partial denture framework challenges the maxillofacial prosthodontists to obtain insight into the intended therapeutic isodosis fields in relation to the strategic important teeth. This sometimes results in a wellconsidered decision to leave teeth which are considered an oral focus of infection in situ (including a thorough discussion of the risk on development of osteoradionecrosis).

With regard to the future prosthodontic rehabilitation, an early decision whether there is a need to place implants is important. This allows for the preferred prosthodontic rehabilitation of head and neck patients. For example, choices in planning, positioning and amount of endosseous oral implants or oncology zygomatic implants are key factors for retention of the prosthetic construction<sup>16,17</sup>. Literature emphasizes the importance of an immediate implant procedure as it has been shown that placement of mandibular implants in edentulous patients during ablative surgery results in a higher number of patients with functioning mandibular dentures after completion of oncologic therapy<sup>2,18,19</sup>. Furthermore, an increasing trend is observed to early complete the prosthodontic rehabilitation for which an immediate implant procedure is often a prerequisite<sup>16,20</sup>. When implants are placed after radiation treatment, the anatomical site where the implants are placed seems to effect implant survival, as the implant survival rate is higher in the mandible than in the maxilla and in grafted bone $2^{1,22}$ . Therefore, implant placement during ablative surgery is preferred, at least in selected cases<sup>16</sup>.

When there is a need for per-operative prosthetics, the maxillofacial prosthodontist has to record the actual intra-oral situation through impression taking, intra-oral scanning and/or cone beam computer tomography (CBCT) imaging, all to capture the intraoral pre-treatment situation and occlusal plane for fabrication of a surgical obturator, surgical guides and models, or an implant-supported prosthesis. A huge advantage of working with three-dimensional (3D) intraoral scanning is the ease to combine the data of the intra-oral situation, like the position of teeth and occlusion, with (CB)CT and magnetic resonance imaging (MRI) data of the surrounding tissues in an augmented model. This 3D virtual model provides more insight into the implications and complexity of surgical and prosthetic rehabilitation. This insight allows the surgical team to analyse the surgical and rehabilitation outcome and plan the treatment $2^{3,24}$ . Although intraoral scan techniques are widely used nowadays, some limitations can occur mostly due to poor intraoral access caused by, e.g., the tumour, trismus or pain. In those situations analogue impressions are the only feasible option. The produced plaster model can then in a second stage be digitallized in order to create the 3D virtual model.

When mutilating extra-oral defects are expected as a result of ablative surgery, extra-oral dimensions have to be recorded as well as to prepare for future extra-oral prostheses . Although analogue workflows still meet the quality standards of prosthetic care, digital technology has demonstrated ease and utility in design and construction workflows in prosthodontics<sup>25</sup>. The prosthodontic documentation can be completed by taking clinical photographs. In this way skin-, prosthetic- and facial characteristics are captured and aid with communication between the head and neck team. With all gathered information a prosthetic draft plan can be worked out in preparation of the necessary input of maxillofacial prosthodontists in choice of rehabilitation treatment.

#### **Multidisciplinary approach**

In the past, prosthodontic rehabilitation in the oncological treatment path was a stand-alone final procedure after completion oncological therapy. Nowadays, planning of surgical reconstruction starting with occlusion of teeth also safeguards a proper dental rehabilitation. This approach supports a thorough adjustment of the surgical and prosthetic planning and treatment before the oncologic treatment is started $23,26$ . In a reconstruction meeting, the head and neck team can go through the available options of surgical, prosthetic or combined reconstruction. The input of maxillofacial prosthodontists in such a reconstruction meeting guards the feasibility from a prosthetic point of view, guided by a prosthetic draft plan, and includes the eventual need for implant placement. With the introduction of 3D planning and computer aided design (CAD) assistance, preoperative virtual augmented models provided by medical engineers at these meetings are a great asset to the surgical team and support shared decision making regarding favourable reconstruction option after oncology treatment.

#### **Virtual planning**

Once the final oncological treatment plan is agreed upon, having access to a preoperative virtual surgical planning (VSP) can be of importance for the surgical team<sup>24</sup>. Three-dimensional planning enables a high accuracy of guided resection surgery and prosthetic driven reconstruction planning<sup>27,28</sup>. Besides a reliable intended outcome, the concept of backwards planning from occlusion maximizes the chances of completing oral rehabilitation of the patient. A 3D VSP can be very precisely executed, with the use of 3D printed guides creating the possibility of completing a full ablative and reconstructive plan in one surgery<sup>23,26</sup>. However, soft tissues are not very reliable reproduced yet by digital techniques. This is still an uncertain factor to be taken into account when it comes to planning prosthetic treatment. The risk of losing prosthetic retention options due to compromised soft tissues means critically assessing choices such as preservation of a functional dental arch (shortened), planning a fixed or removable prosthesis, and indication of peroperative insertion of endosseous oral implants or oncology zygomatic implants. Tools to better reproduce soft tissues are in development.

#### **Rehabilitation of mandibular defects**

Smaller head and neck tumours can require resection of soft tissue only and can surgically be managed by primary closure. To overcome possible absence of vestibule or compromised neutral zone provision of individualized adapted prostheses is required. With such an approach oral function might reach a near normal level after ablative surgery and prosthetic rehabilitation $8$ .

Advanced tumours can result in large defects, requiring surgical reconstruction<sup>29</sup>. The resulting altered anatomy can be unfavourable because of flap positioning and presence of scar tissue. Such unfavourable conditions may impair the ability to speak, masticate and swallow. Loss of sensibility, a shallow or absent buccal vestibule, radiation-induced hyposalivation and trismus may further compromise oral function. Advanced tumour surgery requiring bone resection may further compromise oral function due to loss of the continuity of the mandible, loss of teeth and severe deformities. Most of all, an impaired motility of the tongue challenges the fabrication of a functional mandibular resection prosthesis as it compromises stability of this prosthesis during speech and mastication<sup>30</sup>.

Many of the aforementioned problems can, at least in part, be reduced by the use of endosseous oral implants to retain prostheses (Figure 2). These implants contribute to stabilization of prostheses and reduce loading of the compromised soft tissues and underlying bone<sup>31</sup>. In many patients, an almost normal masticatory function can be achieved with a rehabilitation of the reconstructed side with implant-supported removable partial dental prostheses or implant-retained mandibular overdentures<sup>32</sup>. Maximization of dental rehabilitation significantly improves oral functioning, oral diet achievements and oral health related quality of life<sup>2,33</sup>. Several authors reported that a relatively low percentage of reconstructed patients complete prosthetic rehabilitation<sup>34</sup>. Causes of not completing the prosthetic treatment after implant placement are, vertical discrepancy between the graft and the remaining mandible, which leads to an unfavourable implant–crown ratio, poor quality of soft tissues (hypertrophy often appears after the placement of the abutments), and the type of the prosthesis (fixed or removable)<sup>35</sup>. As implant placement during primary reconstruction shortens the interval between surgery and dental rehabilitation, the number of orally rehabilitated patients will increase<sup>16,36</sup>.



Figure 2. Patient diagnosed with squamous cell carcinoma of the tongue after hemiglossectomy and radial forearm free flap reconstruction.

**a**. Pre-operative image of tumour **b**. Intra-oral view after ablative surgery and postoperative radiotherapy. Bar suprastructure with distal extensions fixed on two endosseous implants **c,d**. Implant supported prosthesis with patient specific design to optimize tongue function during speech and mastication **e**. Orthopantomogram two years after reconstructive surgery showing good integration of endosseous implants.

#### **Rehabilitation of maxillary defects**

Management of maxillary, midface and skull-base tumours is challenging and complex when it comes to ablative surgery with a need for oral and facial reconstruction, and oral rehabilitation. Maxillary resections lead to a variety of oronasal defects, with a diversity of approaches for restoring oral functioning. Manifold maxillectomy classification schemes are mentioned in literature, all originating from the Brown classification published in 2000  $37$ . These schemes categorize the range of maxillary defects by location, extension like the vertical and horizontal components, and biomechanical forces, and provide guidelines for surgical and prosthetic rehabilitation choices**.**

#### *Restorative decision making*

When tumour resection causes a minor oronasal fistula and primary closure is not feasible, surgical reconstruction with soft tissue flaps alone can lead to excellent functional and aesthetic results, as long as prosthetic retention of teeth replacement is guaranteed. For larger maxillary defects, the option of prosthetic rehabilitation with an obturator prosthesis is the standard of care in many institutions since decades<sup>38,39</sup>. This approach includes maxillary obturators for defects of the hard palate, pharyngeal obturators for defects of the soft palate, and maxillopharyngeal obturators for defects that include both structures. However, the discomfort of wearing, removing, and cleaning such a prosthesis, its poor retention in large defects, and the frequent need for readjustments often limit the value of this cost-effective method of restoring speech and mastication<sup>40</sup>.

In case of even larger tumours, the defect size increases and the remaining dentition and supporting palatal bone will be more limited. Due to lack of retention and stability of a prosthesis, the interplay of forces further compromises functional rehabilitation and thereby overall success of treatment<sup>41</sup>. Placing endosseous implants in the native bone of the maxilla will allow to improve retention of the obturator prosthesis and thereby increase the success of prosthetic rehabilitation. Patients with implantsupported obturator prostheses have significantly better masticatory and oral function, and less discomfort during food intake than patients with a conventional obturator $42$ . Studies which compared prosthetic obturation with reconstruction of a palatomaxillary defect demonstrated that there are some advantages to reconstruct the defects above obturation of these defects, in particular with regard to quality-of-life issues such as comfort, convenience, and feelings of self-consciousness<sup>43</sup>. However, especially in medically compromised and older patients, implant-supported obturator treatment is a viable alternative to surgical reconstruction after maxillectomy<sup>42</sup>, although an obturator prosthesis is not obsolete and is still standard care in low-income and middle-income countries. With the benefits of digital techniques and surgical reconstruction options the obturator prosthesis has increasingly gained a temporary function by bridging time to secondary surgical reconstruction of the defect.

New workflows are rising in processing surgical obturators. Several case reports describe production of 3D obturator prostheses<sup>44,45</sup>. 3D knowledge of resection planes provides a better knowledge of the dimensions of the post-resection defect, giving the option of preoperative production of a surgical obturator. With proper tumour visualisation and insight in the remaining anatomic structures, a surgical obturator prosthesis can be digitally designed and printed prior to ablative surgery. A nearby fit can be achieved and only minor per-operative adjustments are needed (Figure 3).

If the defect overextends in size and vertical dimension, obturation of the deffect cannot be adequately addressed with prosthetic management alone<sup>46</sup>. Surgical reconstruction combined with dental rehabilitation is then preferred. Zygomatic implants can, for example , provide a predictable in-defect support for prosthetic rehabilitation of the maxilla if placed at the time of primary surgery<sup>47</sup>. The zygomatic implant perforated flap procedure combines autogenous soft tissue reconstruction with zygomatic implantsupported fixed dental rehabilitation $17,48$ . Furthermore, using the Rohner technique in combination with VSP it is possible to reconstruct high level maxillectomy cases with a reliable single-stage approach (Figure 4) in a secondary stage procedure<sup>26,49-51</sup>.



**Figure 3.** Patient diagnosed with mucoepidermoid carcinoma of the maxilla with prosthetic rehabilitation using a 3D printed obturator prosthesis based on a 3D VSP workflow.

**a.** Tumour visualization based on CT and MRI data fusion related to position of digitalised conventional prosthesis **b.** Virtual design of surgical obturator **c.** Image showing pre-operative printed surgical obturator **d**. Digital designed and printed obturator prosthesis with nearby fit during ablative surgery.



**Figure 4.** Jaw reconstruction of patient diagnosed with ameloblastoma treated with maxillectomy and reconstruction with fibular free flap.

**a.** the tumour was delineated on the MRI using radiotherapeutic planning software **b.** 3D VSP for tumour ablation surgery **c.** Virtual surgical planning of the maxilla and orbital floor reconstruction with fibula bone and implant planning. **d.** Suprastructure fixed on 2 endosseous implants placed in the fibula bone segment. **e.** Orthopantomogram four years after reconstructive surgery showing good integration of fibula bone segment and implants.

#### **CONCLUSION**

Oral rehabilitation is an encompassing component of the treatment of head and neck cancer patients and is a major contributor to enhance the quality of life of cancer survivors. Involvement in a multidisciplinary team to prepare and excecute the rehabilitation treatment is of utmost importance. Maxillofacial prosthodontists should be involved from the beginning, their role in this process is essential and guiding. The rise of 3D techniques in diagnostics, planning and oral rehabilitation is enormous, and is expected to evolve to the standard of care.

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## **CHAPTER**

# 2.2

**What is the optimal timing for implant placement in oral cancer patients? A scoping literature review**

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*This chapter is an edited version of the manuscript: What is the optimal timing for implant placement in oral cancer patients? A scoping literature review*

Oral Diseases 2021;27(1):94-110.

#### **ABSTRACT**

#### **Background**

Oral cancer patients can benefit from dental implant placement. Traditionally implants are placed after completing oncologic treatment (secondary implant placement). Implant placement during ablative surgery (primary placement) in oral cancer patients seems beneficial in terms of early start of oral rehabilitation and limiting additional surgical interventions. Guidelines on the ideal timing of implant placement in oral cancer patients are missing.

#### **Objective**

To perform a scoping literature review on studies examining the timing of dental implant placement in oral cancer patients and propose a clinical practice recommendations guideline.

#### **Methods**

A literature search for studies dealing with primary and/or secondary implant placement in Medline was conducted (last search December 27<sup>th</sup>, 2019). The primary outcome was 5-year implant survival.

#### **Results**

16 out of 808 studies were considered eligible. Both primary and secondary implant placement showed acceptable overall implant survival ratios with a higher pooled 5-year implant survival rate for primary implant placement 92.8% (95% CI: 87.1%-98.5%) than secondary placed implants (86.4%, 95% CI: 77.0%-95.8%). Primary implant placement is accompanied by earlier prosthetic rehabilitation after tumour surgery.

#### **Conclusion**

Patients with oral cancer greatly benefit from, preferably primary placed, dental implants in their prosthetic rehabilitation. The combination of tumour surgery with implant placement in native mandibular bone should be provided as standard care.

#### **INTRODUCTION**

The general treatment timeline for oral cancer patients consists of diagnostics, surgical treatment followed by postoperative (chemo)radiation therapy depending on the surgical margins and specific tumour properties, or solely (chemo)radiation therapy. Traditionally, oral rehabilitation comes last, i.e., after the oncologic treatment when the oral mucosa is completely healed (Figure 1). Oral function after treatment for a malignancy in the oral cavity is often compromised due to changed anatomy after surgery and/or the oral sequelae of radiotherapy like xerostomia and trismus $1/2$ . Sometimes teeth need to be extracted during ablative surgery because of their location in proximity to the tumour or as part of a pre-radiation screening examination<sup>3</sup>. This compromised oral condition also leads to a decrease in oral function and possible a negative effect on nutritional status and quality of life<sup>4</sup>. Fabrication of functional prostheses, frames and conventional partial dentures is often difficult to achieve after oncologic treatment and in some cases even impossible<sup>5,6</sup>.



Combined oncologic treatment & rehabilitation phase	
<b>Oncologic treatment and implant placement</b>	<b>Oral rehabilitation</b>
Surgical treatment and implant placement - Postoperative (chemo)radiation therapy	<b>Prosthesis placement</b>

**Figure 1.** Timing of oncologic treatment and oral rehabilitation.

Dental implants have shown to be a great asset in oral cancer patients and provide good results<sup>7,8</sup>. When dental rehabilitation based on implants first was introduced in oral cancer patients, they were often placed after oncologic treatment (secondary implant placement)<sup>9</sup>. This implies an additional surgery, for irradiated patients under antibiotic prophylaxis, and an additional treatment burden in older patients with often multiple comorbidities. When pre-treatment hyperbaric oxygen treatment is advised, the treatment burden increases even more $10$ . When offering implant treatment in a secondary phase, patients are less likely to accept or undergo additional procedures, even when they could benefit from an implant supported prosthesis $7,11$ .

Implants can also be placed during tumour surgery (primary implant placement) $^{12}$ . An advantage of this treatment sequence is that most of the osseointegration takes place during the recovery phase, saving the burden of additional surgery and a considerable amount of time. The patient can function with an implant-supported prosthesis much earlier after completion of oncologic treatment<sup>6</sup>. Disadvantages are possibly improper placement of implants due to the changed anatomy during surgery or the risk of implants not being used because of tumour recurrence or patients passing away before a prosthesis can be made (loss of resources). The effects of radiotherapy on the osseointegration process and implant survival rates are also subject of debate and primary implant placement is not always available in the hospital setting<sup>13-15</sup>.

Guidelines when to ideally start oral rehabilitation with dental implants in oral cancer patients are lacking. Several systematic reviews have been published, mainly dealing with timing of secondary implant placement after radiotherapy<sup>16-20</sup>. Claudy et al. (2013) reported that dental implant placement between 6 and 12 months after radiotherapy was associated with a 34 % higher risk of failure and therefore suggest waiting periods over 1 year after radiotherapy<sup>17</sup>. On the contrary, it has been suggested that implant placement just becomes more critical over time because of the ongoing progressive decrease in healing capacity of bone after radiotherapy<sup>21</sup>. Other studies showed no significant relationship between time interval and dental implant survival rates $18,20$ . The implant survival rate in patients with a history of radiotherapy seems to be more associated with the location of the implants (more implant loss in the maxilla than in the mandible) than with the of time after radiotherapy<sup>22</sup>. Far less studies on primary implant placement have been published. A systematic review by Barber et al. (2011) on primary implant placement provides an extensive literature overview, but no clear conclusions or recommendations were made<sup>23</sup>. The latter systematic review also included case reports and studies on patients with benign lesions, which could have influenced the outcome. The authors of another systematic review highlighted the importance of timing of implant placement and concluded that they could not extract scientific evidence for the optimal timing of implant placement<sup>15</sup>.

Before being able to propose guidelines for optimal timing of implant placement in head and neck cancer patients needing radiotherapy, the following questions have to be answered: (1) what is the optimal timing of dental implant placement in oral cancer patients with regard to implant survival and functional outcomes, and (2) can all oral cancer patients benefit from primary placement or is this method of treatment only suitable for specific patient groups. As implant treatment and techniques have evolved during the last decade, we comprehensively reviewed the literature on the timing of implant placement in oral cancer patients to compose recommendations for clinical practice with regard to optimal timing of implant placement in this category of patients.
# **METHODS**

A search was conducted in MEDLINE (from 1995 through October 16<sup>th</sup> 2019) on October 16th 2019 according to the syntax rules of the database. Key words and their combinations were used to identify relevant studies (Table 1). The titles and abstracts from all the searches were reviewed.

Inclusion criteria were studies published in English regarding primary or secondary implant placement in oral cancer patients, cohort studies, case-control studies, (randomized) controlled trials. Review articles, animal studies, case reports, case series with less than 10 patients and studies regarding extra-oral craniofacial implants were excluded. When it was not clear from the title and abstract if the paper dealt with implant placement in the upcoming irradiated (primary implant placement) or already irradiated (secondary implant placement) mandible or maxilla, the full text was reviewed and the article was included or excluded. 41 full-text articles were assessed followed by exclusion of 26 articles due to various reasons (Figure 2). Furthermore, hand searches of the references of retrieved articles were carried out. The search was updated on December 27th 2019 and one additional article was included. Eventually 16 studies were included.



#### **Table 1.** Search strategy

### **Data extraction**

The following data were collected from the studies: patient demographics (age, oncologic diagnosis, patients' dental status before treatment), type of oncological treatment, timing of endosseous or zygomatic implant placement (primary, secondary), implant system, site of implant placement, type of tissue implants were inserted into (native or augmented bone), time until loading, implant loss, implant survival ratios, complications, perioperative measurements, type of prosthesis and follow-up period (Tables 3.1-3.3). When available, the time span between (implant) surgery and prosthesis placement, and the time between radiotherapy and secondary implant placement was recorded.

### **Statistical analysis**

Quantitative data-synthesis was performed for the studies reporting 5-year dental implant survival rates of primary placed implants and secondary placed implants. Studies which did not report on the 5-year implant survival rate were not included in the quantitative analysis. The pooled 5-year implant survival rates were analyzed using a random effects model. Analyses were performed with Comprehensive Meta-Analysis software, Version 3 (CMA, Biostat, Englewood, NJ 07631, USA).



**Figure 2.** Flowchart of study selection procedure

# **RESULTS**

16 out of 808 papers were considered eligible for our study and one additional article was included after updating the search (Figure 2). These 16 studies provided data on a total of 4449 implants, of which 753 implants were placed in grafted bone (osseous free flaps). The majority of studies (68.8%) had a retrospective design. Preoperative dental status (edentulous or dentate) was not always reported. Patients received an implant supported removable or fixed prosthesis. A variety of malignancies in the head and neck region was reported. Oncologic treatment consisted of tumour surgery in addition to radiotherapy. Three articles reported on including patients who were treated with chemotherapy<sup>11,24,25</sup>. Eight articles reported solely on secondary implant placement<sup>11,24,26-31</sup>, two studies described patients with only primary placed implants<sup>32,33,34</sup> and six articles described both primary and secondary implant placement<sup>25,34-38</sup>. In all studies implants were placed in a 2-stage manner. When mentioned, the number of implants per patient ranged between 2 to 4 in the interforaminal region of the mandible $32-34,36$ . Only one study reported the number of implants placed in the maxilla  $(3$  to  $5)^{29}$ . From the available data, a total of 987 implants were placed in the maxilla and 131 zygomatic implants were placed in the zygomatic bone.

### **Implant survival**

The pooled 5-year survival rate for primary placed implants was 92.8% (95% CI: 87.1%- 98.5%) (Figure 3), while the pooled implant survival rate for secondary placed implants was 86.4% (95% CI: 77.0%-95.8%) (Figure 4). The 5-year implant survival rate of primary placed implants tended to be higher compared to secondary placed implants. Survival ratios for dental implants placed in vascularized bone grafts varied between 54 and 93.8% (Table 3.2). The implants in vascularized bone grafts were placed in a secondary procedure. Implant survival ratios in native maxillary bone ranged between 57.1 and 95.3%. One study focused mainly on zygomatic implants (Butterworth 2019) and reported a 5-year implant survival rate of 92%.



**Figure 3.** Forest plot for cumulative weighted 5-year implant survival rate for primary implant placement.



**Figure 4.** Forest plot for cumulative weighted 5-year implant survival rate for secondary implant placement.

## **Time between ablative surgery, implant placement, radiotherapy and prosthesis placement**

In two studies on primary implant placement, a healing period of 6 months after radiotherapy was applied before second stage surgery<sup>33,38</sup>. In another study a waiting period of 9 months was applied<sup>32</sup>. Time from tumour surgery and implant placement until prosthesis placement from 3 studies varied from 6.3 to 21.4 months $33,36,38$ .

In the secondary setting there was a preference for waiting at least six months after completing radiotherapy before starting implant treatment. Some studies even preferred to wait at least 1 year<sup>34,36</sup>. Generally, patients had to wait more than one year after oncologic treatment before the oral rehabilitation was started. In the article by Flores-Ruiz et al. (2018) 70% of the patients started with implant therapy even later than 2 years after oncologic therapy<sup>11</sup>. The study of Seikaly et al. (2019) reported a mean time to prosthetic rehabilitation of 73.1 months $^{38}$ . For zygomatic implants there was also a difference between primary and secondary placed implants (median time until loading 1.7 months versus 9.3 months $3^3$ .

### **Functional outcomes**

Korfage et al. (2014) described that irradiated patients experience more limitations in oral function than those who were not<sup>33</sup>. Chewing ability decreased over time in irradiated patients, but there was still a better oral function in patients with a prosthesis than in patients without a prosthesis<sup>33</sup>. A more objective method for measuring oral function was applied in the study by Wetzels et al. (2016) by determining masticatory performance34. The authors showed an increased masticatory performance in all patients with implant-supported prostheses, supporting the assumption that implants are beneficial for improved oral function in oral cancer patients.

### **Complications**

Intra- and postoperative complications of dental implant placement were uncommon. The most common reported complication was osteoradionecrosis (ORN) in irradiated patients25,33-35. The ORN rate varied between 1.8 and 7.7%. One study reported a pathologic fracture, but it was unclear if the fracture occurred because of implant placement<sup>25</sup>. In the study with zygomatic implants, infection of the overlying skin in secondary placed implants occurred in 2 patients<sup>37</sup>. There were no complications in the group with primary placed zygomatic implants. Other complications like wound infections, wound breakdown and partial fibular skin graft loss were described for implants placed in fibula free flaps<sup>38</sup>. Technical complications in primary and secondary placed implants included incorrect implant positioning. In the study of Korfage et al (2014), 6 out of 164 patients (3.7%) with primary placed implants did not receive an implant supported prosthesis due to incorrect implant positioning<sup>33</sup>. Another study reported 17.7% unused implants after primary placement (17.7%) due to incorrect positioned implants and tumour related factors<sup>36</sup>.

## **DISCUSSION**

Timing of dental implant placement in oral cancer patients is a subject of continuing debate. Although most of the studies that were considered to be eligible for the review had retrospective study designs and studied implant placement in heterogeneous patient populations, it can be concluded that dental implant placement, irrespective of the timing of implant placement, is a reliable treatment option for head and neck cancer patients. Both primary and secondary implant placement show an acceptable overall implant survival. Comparison between both groups showed a tendency for a higher 5-year implant survival rate in primary implant placement. This trend, however, did not reach statistical significance. Implants placed in the maxilla tended to have lower survival ratios than implants placed in the mandible. The lower implant survival ratios in maxillary bone might be related to the thinner cortical bone of the maxilla. For zygomatic implants however, 5-year implant survival rates of 92% were reported<sup>37</sup>. An explanation for these favourable outcomes could be that zygomatic implants are inserted in highly cortical bone of the zygoma, leading to a high initial stability. Because of their length, these implants may also be situated outside of the radiated field, therefore avoiding toxic radiation dosages. At this moment, functional results for zygomatic implants seem good and complication rates low, but guidelines on the optimal workflow are not yet available<sup>39</sup>.

A great advantage of primary implant placement is the earlier prosthetic rehabilitation after tumour surgery. The latter is a great asset, also because it is not uncommon that head and neck cancer patients refuse the burden of undergoing the secondary implant placement, notwithstanding the great advantage they could experience from an implant-supported oral rehabilitation<sup>7</sup>.

The costs and potential 'loss of resources' from implants not being used is an important issue in primary implant placement. The percentage of incorrect placed implants varied between the studies. We believe that with the help of 3D-technology, implant positioning (especially in difficult cases) can be further improved as has already been demonstrated in small groups for primary implant placement<sup>40</sup>. Placing implants during ablative surgery slightly lengthens the operating time, but the extra costs and burden to the patient of an additional secondary implant procedure under local anesthesia are prevented.

As stated earlier, precision of implant placement can be improved further with 3D-technologies or surgical design and simulation (SDS). In both primary and secondary implant placement 3D-planning software can be used to assess the amount of available bone height and width for dental implants after resection and to assess the ideal location for the implants from a prosthetic point of view<sup>41</sup>. The use of SDS has resulted in a high percentage of implant utilization (96%) for mandibular defects constructed with fibula free flaps<sup>38</sup>. We therefore consider the availability of 3D-planning techniques a necessity in the reconstruction of oral cancer patients with complex (continuity) defects.

Only one study on primary implant placement in osseous free flaps for larger defects was considered eligible for our review<sup>38</sup>. In this prospectively conducted study, dental implants were placed in bone grafts (mainly fibula grafts) during the ablative procedure. This resulted in a significant reduction of time to rehabilitation and percentage of patients rehabilitated. Most reports on implant placement in osseous free flaps include heterogeneous patient populations and show successful treatment outcomes with implant survival ratios between 80 to  $100\%^{42,43}$ . Jackson et al. (2016) compared primary to secondary implant placement in fibula free flaps and found no difference in implant survival between primary and secondary implantation, and between nonirradiated and irradiated patients<sup>44</sup>. The 1-year results of Sandoval et al. (2019) in 10 patients with primary placed implants in fibula free flaps show that the presence of dental implants in fibula free flaps does not lead to more postoperative complications or an increase of radiotherapy related toxicities<sup>45</sup>. Despite these promising results, correct placement of dental implants in osseous free flaps during ablative surgery is technically challenging as reviewed by Bodard et al.  $(2011)^{46}$ . One way of partially reducing these challenges is through the use of occlusion-driven reconstructions aided by 3D-planning, as is demonstrated in the article of Seikaly et al. (2019)<sup>38</sup>. However, the essential difference in tissues covering the grafted bone of the fibula and native mandibular bone remains. The presence of subcutaneous tissue and the absence of keratinized gingiva could affect implant survival and peri-implant health. The patients should be strictly monitored to see whether complications might occur on the long run. Additional thinning or correction of the overlying skin paddle is sometimes necessary during second stage surgery<sup>42,47</sup>. Regarding functional outcomes, Wijbenga et al. (2016) concluded from their systematic review that despite high implant survival ratios, it is not possible to state what the effect of implant-supported dental prostheses is after reconstruction with a fibula free flap, again mainly due to the diversity of methods used to assess functional outcomes<sup>47</sup>. Awad et al. (2019), however, concluded in their systematic review that 61% of patients with a vascularized fibula flap receiving dental rehabilitation reported good oral function and was able to consume a normal diet<sup>48</sup>. The latter authors, however, did not make a statement on the timing of implant placement in vascularized fibula flaps. With respect to timing of implant placement in osseous free flaps, it is generally advised to insert implants primarily only in patients with benign lesions $47,50$ . In our clinic we prefer to place dental implants as much as possible in the remaining native mandibular bone (during ablative surgery) in order not to jeopardize the vitality of the vascularized fibula flap. As mechanical stability comes from the more anterior region of the mandible, this approach is successful in lateral and antero-lateral defects.

Limitations of this scoping review include, as stated earlier, the retrospective study designs, heterogeneous patient populations, exclusion of non-English papers, the use of one database and the fact that screening by carried out by assessor. These factors could result in bias. Due to the unavailability of large prospective studies on the timing of implant placement in oral cancer patients, the treatment of choice will mainly depend on surgeon experience and preference. However, based on the findings in the current study and our own experience in treating these patients, we composed treatment recommendations on the timing of implant placement in patients with malignant intraoral tumours (Table 2). We realize that these recommendations may not be applicable to all hospital settings as 3D-planning software and the financial resources for primary implant placement may not be available in every centre.



\*Includes zygoma implants

**Table 2.** Recommendations for dental implant placement to support implant-retained overdentures in head and neck cancer patients*.*

# **CONCLUSION**

Based on the studies included in this review, as far as the timing of implant placement is regarded, we propose to routinely combine tumour surgery with implant placement in native mandibular bone as standard care (primary implant placement). The functional benefits of primary implant placement outweigh the risk of leaving (some) implants unused. For more complex reconstructive cases, a personalized treatment approach (aided by 3D-technologies) is necessary and is more often in need of a secondary implant placement. It seems that primary placement of zygomatic implants is accompanied by a high implant survival and good oral rehabilitation although more research is needed on this particular topic.

### **Conflict of interest**

The authors have stated explicitly that there are no conflicts of interest in connection with this article.



What is the optimal timing for implant placement in oral cancer patients? A scoping literature review

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IMRT: intensity-modulated radiation therapy, HBO: hyperbaric oxygen; BI: bleeding index; GI: gingiva index; PI: plaque index, Gy: Gray; AB: antibiotic; EORTC RT: radiotherapy; SCC: squamous cell carcinoma; ACC: adenoid cystic carcinoma; ORN: osteoradionecrosis, FFF: fibula free flaps. PORT: postoperative radiotherapy; RT: radiotherapy; SCC: squamous cell carcinoma; ACC: adenoid cystic carcinoma; ORN: osteoradionecrosis, FFF: fibula free flaps. PORT: postoperative radiotherapy; IMRT: intensity-modulated radiation therapy, HBO: hyperbaric oxygen; BI: bleeding index; GI: gingiva index; PI: plaque index, Gy: Gray; AB: antibiotic; EORTC QLQ: European Organization for Research and Treatment of Cancer Quality of Life Questionnaire; OHIP: Oral Health Impact Profile. QLQ: European Organization for Research and Treatment of Cancer Quality of Life Questionnaire; OHIP: Oral Health Impact Profile.

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# **CHAPTER**

**The use of 3D virtual surgical planning and computer aided design in reconstruction of maxillary surgical defects**

2.3

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*This chapter is an edited version of the manuscript; Current opinion in Otolaryngology & Head and Neck Surgery 2020;28(2):122-128.*

# **ABSTRACT**

### **Purpose of review**

The present review describes the latest development of 3D virtual surgical planning (VSP) and computer aided design (CAD) for reconstruction of maxillary defects with an aim of fully prosthetic rehabilitation. The purpose is to give an overview of different methods that use CAD in maxillary reconstruction in patients with head and neck cancer.

### **Recent finding**

3D VSP enables preoperative planning of resection margins and osteotomies. The current 3D VSP workflow is expanded with multimodal imaging, merging decision supportive information. Development of more personalized implants is possible using CAD, individualized virtual muscle modelling and topology optimization. Meanwhile the translation of the 3D VSP towards surgery is improved by techniques like intraoperative imaging and augmented reality. Recent improvements of preoperative 3D VSP enables surgical reconstruction and/or prosthetic rehabilitation of the surgical defect in one combined procedure.

### **Summary**

With the use of 3D VSP and CAD, ablation surgery, reconstructive surgery, and prosthetic rehabilitation can be planned preoperatively. Many reconstruction possibilities exist and a choice depends on patient characteristics, tumour location and experience of the surgeon. The overall objective in patients with maxillary defects is to follow a prostheticdriven reconstruction with the aim to restore facial form, oral function, and do so in accordance with the individual needs of the patient.

### **Keywords**

3D VSP, CAD/CAM, maxillary, oral rehabilitation, patient specific, reconstruction

### **Key points**

- Successful dental rehabilitation after maxillary ablative surgery is a complex, multidisciplinary team effort
- The overall objective in patients with maxillary defects is to follow a dental rehabilitation driven reconstruction with the aim to restore facial form and oral function, in accordance with the individual needs of the patient.
- Integration of multi-modality imaging into a single 3D VSP improves the predictability, accuracy and speed of surgical procedures.
- The design of patient specific implants should be optimised using patient specific finite element analysis and topology optimization.

# **INTRODUCTION**

Surgical treatment of tumours located in the maxilla can be a challenge because of anatomical constraints and impairment of function following treatment. With the introduction of 3D virtual surgical planning (VSP) and guided surgery techniques, complex resections can be planned preoperatively and can be combined with reconstructive solutions. Advantages of using 3D VSP becomes apparent in the operating room as decisions regarding resection margins, location of osteotomies, precise placement of osteosynthesis materials and dental implants are already decided upon before the surgery. Because of the high accuracy of 3D VSP, surgical resections with good tumour margin control can be obtained during ablation $1/3$ . Moreover, it enables the use of bone containing multi-segment composite flaps and/or dental implants in one combined ablative and reconstructive procedure.

Therefore, 3D VSP and guided surgery is the current standard in head and neck oncologic surgery. Another form of computer-assisted surgery (CAS) includes surgical navigation. Surgical navigation is already routinely used during maxillary tumour resections and reduces tumour positive resection margins compared to conventional surgery $4.5$ . VSP has been shown to be cost-effective, reproducible, accurate and opens possibilities for creative patient-specific (PS) solutions<sup>6-9</sup>.

The aim of this manuscript is to provide an overview of current state of the art routines for using 3D VSP in maxillary ablative surgery, reconstruction and dental rehabilitation. In addition, indications for expected developments in the field of 3D VSP and optimization of patient-specific implants are described.

### **Resection and reconstruction of maxillary defects**

Resection of neoplasms in the maxilla often result in complex defects encompassing soft tissue, bone and dentition. This results in diminished aesthetics and impaired oral functions and thereby lowers the quality of life perceived  $1-d$ . The aim of reconstruction of maxillary and midfacial defects should be to restore form and function with minimal operative morbidity.

A variety of different single-stage reconstructive techniques in midfacial defects are used. The use of a classification system describing midfacial defects can be helpful in determining reconstructive options  $5-10$ . The classification of Brown et al. is the most widely recognised classification <sup>5</sup>. Despite these popular classification systems, they describe the defect focusing only on its reconstructive possibilities <sup>11</sup>. Often, defects do not fit in a particular classification, or the classification schemes do not take dental rehabilitation or patient factors in consideration <sup>11</sup>.

The reconstructive ladder is a heuristic approach to reconstruction, in which the simplest and safest approach to a problem is often the preferred solution  $12$ . Taking the reconstructive ladder in consideration is important to manage maxillary and midfacial defects <sup>11</sup>. Small defects can therefore be closed by local flaps such as the buccal fat pad flap or temporalis muscle flap, especially if these are located laterally in the posterior maxilla  $6,8,11,13$ . If defects limited to the palate are present and retention is possible, obturator prosthesis can be a very good option  $11$ . These obturators remain a simple, non-surgical and relatively quick approach which offers immediate improvement of oral functions with reasonable outcomes. However, obturator prostheses have several drawbacks regarding oral hygiene, instability, velopharyngeal insufficiency, lack of soft tissue support and they carry a social stigma 13,14. With larger defects the use of pedicled or free vascularised autologous tissue transfer can offer skin, muscle, fascia and bone and can be used as a foundation for dental implants  $^7$ .

Bony reconstruction is not always necessary as retention of a prosthesis can be found on canines and incisors or zygomatic implants can be placed in these defects <sup>7</sup>. The most used autologous reconstruction method of a maxillary defect involving alveolus and maxillary sinus wall, is the radial forearm free flap (RFFF) <sup>5</sup>. The fibular free flap (FFF), Iliac crest or deep circumflex iliac artery (DCIA) and the subscapular system are the most used composite flaps in maxillary reconstruction when bone is required  $7.11$ . The FFF is the most often used, as it can be reliably harvested and transferred, its bone stock enables reliable placement of implants, has a long vascular pedicle, high success rate, low donor site morbidity and it enables a simultaneous two team approach  $7.15$ . A DCIA flap offers bigger amounts of muscle and bone that has a contour better suited to reconstruct the most complex defects encompassing loss of all 6 walls of the maxilla 16,17. Large complex defects that need multiple skin paddles, muscle and bone can be reconstructed by flaps based on the scapular system 18–20.

## **Dental rehabilitation**

Oral functions are not only dependent on reconstruction of the maxillary defect since, after postoperative radiotherapy, stability and retention of a prosthesis are also decreased 15. Therefore, implants to support prostheses are widely used as part of a standard oral rehabilitation plan <sup>21-24</sup>.

Dental rehabilitation is an essential part of the aim of reconstruction and should be planned from the beginning  $6.25$ . From a prosthodontics perspective CAD assistance benefits the functional outcome. Prosthetic driven reconstruction planning in combination with precise guided placement of dental implants carried out at time of tumour resection ahead of possible radiotherapy is a huge advantage for accelerating the process of oral rehabilitation <sup>26,27</sup>.

As an alternative for bone reconstruction with regular dental implants, zygomatic oncology implants can also provide a predictable in-defect support for prosthetic rehabilitation of the maxilla and can be placed at the time of ablative surgery  $28-30$ . The zygomatic implant perforated flap procedure combines autologous soft tissue reconstruction with zygomatic implant-supported dental rehabilitation 31,32. However, the limited intraoperative visibility makes accurate placement of the zygoma implants challenging. The use of 3D VSP and guided placement by means of 3D printed drilling and placement guides can possibly improve the success in terms of accuracy. Such 3D VSP workflow is illustrated in Figure 1, where a traditional obturator prosthesis is replaced for zygomatic implants. Sometimes zygoma implants cannot provide satisfactory anchorage due to insufficient bone volume and composite free flaps are not indicated. In those patients, an alternative to achieve oral rehabilitation is to design patient specific subperiosteal implants  $33,34$ . An example of such 3D VSP workflow including the design of a patient specific implant is seen in Figure 2.





Obturator prostheses maintain their importance in rehabilitation by bridging time to secondary surgical reconstruction of the defect. Preoperative 3D knowledge of resection planes induce new and more efficient workflows in processing surgical obturators. Several case reports describe production of 3D obturator prostheses with the advantage that they can be printed hollow and aligned to the contour of the patients' defect  $35-39$ . Figure 3 shows an example of a 3D VSP including guided tumour resection and a CAD/ CAM manufactured obturator prosthesis.



**Figure 2.** 3D VSP and CAD workflow of a patient specific subperiosteal implant for secondary reconstruction following maxillary resection. Surgical reconstruction with composite flaps or placement of zygomatic oncology implants was not feasible. The aim of the 3D VSP was to obtain an optimal dental rehabilitation using backwards planning, starting with an optimal position of the prosthesis. **A.** Patient after maxillary resection with non-functional obturator prosthesis **(grey),** fixated by zygomatic wires. **B**. 3D VSP of ideal prosthetic position using a 3D reconstruction of the pre-ablative CT scan of the maxilla **(purple). C.** 3D visualisation of sub-periosteal implant (**green)** in relation to 56Gy isodosis radiotherapy field **(red).** The PSI sub-periosteal implant was designed with the position for fixation screws circumventing the irradiated bone. **D.** Implant strength and fatigue resistance was calculated using finite element analysis to withstand reported maximum occlusal loading. **E.** Planned prosthetic outcome **(grey)** and prosthetic driven sub-periosteal implant position **(green).**

### **Virtual surgical planning and future perspectives**

3D VSP and 3D printed cutting guides are used for complex reconstructive surgery including FFF and DCIA transplantations, combined with one stage implant placement for dental rehabilitation. Currently, in most cases 3D VSP and guided surgery is primarily based on computer tomography (CT) data only. 3D VSP enables planning of oncologic resections and reconstructions using computer-aided design and manufacturing (CAD/ CAM) of 3D printed anatomical models, surgical guides and patient specific implants 27,33,34,40,41. Recent improvements in 3D VSP and CAD workflows include the use of multimodal data fusion to increase precision of determining the tumour free resection margin. Data fusion of MRI and CT enables tumour information delineated on the MRI in spatial relation with bone information from CT. The combination of information provided by CT and MRI with regard to localisation, size and shape of the tumour is important for a precise resection  $42,43$ . An example of such 3D VSP workflow including MRI and CT data fusion is seen in Figure 3. This workflow applied in mandibular tumours provided a tumour free bone resections without per- operative deviation of the 3D VSP<sup>44</sup>. Tumour free resection margins are critical for one stage reconstruction surgery, where the reconstruction is preoperatively planned. An equivalent software pathway can be used for a variety of imaging data, like adding PET data when MRI information is inconclusive about the tumour margin  $45-47$ . Another recent advancement of data fusion is that of CT and radiotherapy dose. Adding radiation dose as a visual volume in the VSP workflow enables evaluation of prescribed radiation dose on tissue and avoiding areas at risk for osteoradionecrosis in patients which were previously irradiated <sup>48–50</sup>. Both 3D

VSP workflows illustrated in Figures 1 and 2 incorporated data fusion of the radiation dose for implant planning and design, including screw locations.

When a 3D VSP is completed and agreed on by the multidisciplinary surgical team, patient specific 3D cutting and drilling guides and patient specific osteosynthesis are designed and used for translation into the surgical procedure. The design of these patient specific guides is adapted to the contour of the bone to achieve the precise resections and drill holes as intended in the VSP. An alternative method of translating the 3D VSP into the surgical procedure, is intra-operative navigation, especially used in case of maxillary resection  $51,52$ . Compared to intra-operative navigation, 3D fitted guides lead to the most accurate bone resections  $27,53-55$ . However, per-operative imaging and navigated surgery enables the surgeon to act on tissue volume changes between preoperative imaging and surgery, in contrary to the 3D fitted premade guides. With the increase of hybrid OR applications (ability of perioperative MRI and CT imaging), one can expect multimodal data fusion real-time in the operating room, updating the preoperatively made 3D VSP with recent per operative imaging data. Intraoperative imaging combined with surgical navigation is reported to be as accurate as the use of 3D printed guides 56.

The main drawback of navigation systems is that the surgeon has to look away from the surgical field in order to receive feedback from the navigation system, this leads to more difficult eye-hand coordination <sup>57</sup>. Augmented reality (AR) could potentially overcome this problem by translating 3D VSP to the actual surgical field with the use of head mounted devices<sup>58</sup>. Preliminary studies report on application of AR for mandibular osteotomies and orthognathic surgery, however the added benefit for maxillary tumour resection and reconstruction has not yet been demonstrated 54,58,59.



**Figure 3.** Tumour visualisation based on CT and MRI data fusion. CT images are used for 3D reconstruction of bone tissue, while the MRI enables delineation of the tumour. This enables preoperative planning of the bone resection **(blue)** and thereby guide design **(grey).** Pre-operative CAD/CAM manufactured obturator prosthesis **(green)** designed to obturate the defect following guided resection.

Design and fit of 3D guides and osteosynthesis materials has to be adapted to the patient bony contour to be used in implementing the VSP into the patient. 3D printed patient specific anatomical models have been used for bending of the shelf osteosynthesis materials like titanium meshes and reconstruction plates. While bending a titanium mesh on a PS model can lead to postoperative facial symmetry and successful clinical outcomes in maxillary reconstructions, complications can include exposure of the osteosynthesis material 49,50.

Designing and using patient specific osteosynthesis materials has shown to be a valuable tool in the reconstruction of oncologic defects, enabling planning of adaptation of implant and screw location, based on the thickness of the bone 27,33,34,40,49,60. Furthermore, possible surgical access can be taken into account. Mostly tailoring of osteosynthesis starts with adapting conventional plate designs and is based on experiences of the involved surgical team and technical physicians. This design process mostly lacks a systematic application of biomechanical analysis on an individual patient basis. It is reported that these osteosynthesis used for mandibular reconstruction can be subject to failure in terms of plate fracture or screw loosening, however comparable complications occur for maxillary reconstructions  $61,62$ . Although patient specific osteosynthesis have been used regularly, future applications should focus on a more patient tailored approach, using 3D print technology. In this way, nearly every shape of osteosynthesis material can be produced. Therefore an approach of more biomechanically based patient specific designs is the logical next step. Based on individual models including bone morphology, bite forces and anatomy a PSI is designed and manufactured. Pilot-studies have demonstrated validation of virtually modelling the muscles associated with mastication  $63$ . Those and other models can be used as a foundation for finite element analysis (FEA). Application of finite element models can predict behaviour of osteosynthesis materials with varying inputs of muscle forces, loads, constraints and biomechanical properties of bone. The output of FEA can be used for topology optimisation, whereby the design, structure and layout of patient specific osteosynthesis can be optimized 64. In addition new materials and surface finishes should be incorporated in the PSI in order to reduce scattering on post-operative imaging and reduce occurrence of infections.

# **CONCLUSION**

Successful rehabilitation after ablative surgery of the maxilla can be achieved through the experience and good collaboration of a multidisciplinary surgical team. The role of a technical physician enabling 3D virtual surgical planning and visualisation of the complex reconstruction of large maxillary defects is of great importance. Preoperative planning enables combined ablation surgery with prosthetic driven reconstruction treatment that benefits the functional outcome. The method of reconstruction is dependent on
many factors like size and location of defect, medical condition, patient factors and previous treatments. In reconstruction of maxillary defects, the use of CAD enables a pre-planned precise, efficient and patient specific treatment with incorporation of dental rehabilitation.

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# **CHAPTER**

**Immediate implant-retained prosthetic obturation after maxillectomy based on zygomatic implant placement by 3D guided surgery: a cadaver study**

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*This chapter is an edited version of the manuscript: Immediate implant-retained prosthetic obturation after maxillectomy based on zygomatic implant placement by 3D guided surgery: a cadaver study.*

International Journal of Implant Dentistry 2021; 14;7(1):54.

\* Shared first authorship.



## **ABSTRACT**

#### **Background**

The aim of this study was to introduce a complete 3D workflow for immediate implant retained prosthetic rehabilitation following maxillectomy in cancer surgery. The workflow consists of a 3D virtual surgical planning for tumour resection, zygomatic implant placement, and for an implant-retained prosthetic-obturator to fit the planned outcome situation for immediate loading.

### **Materials and methods**

In this study, 3D virtual surgical planning and resection of the maxilla, followed by guided placement of 10 zygomatic implants, using custom cutting and drill/placementguides, was performed on 5 fresh frozen human cadavers. A preoperatively digitally designed and printed obturator prosthesis was placed and connected to the zygomatic implants. The accuracy of the implant positioning was obtained using 3D deviation analysis by merging the pre- and post-operative CT scan datasets.

#### **Results**

The preoperatively designed and manufactured obturator prostheses matched accurately the per-operative implant positions. All five obturators could be placed and fixated for immediate loading. The mean prosthetic point deviation on the cadavers was  $1.03 \pm 0.85$  mm; the mean entry point deviation was  $1.20 \pm 0.62$  mm; and the 3D angle deviation was 2.97 ± 1.44°.

#### **Conclusions**

It is possible to 3D plan and accurately execute the ablative surgery, placement of zygomatic implants, and immediate placement of an implant-retained obturator prosthesis with 3D virtual surgical planning. The next step is to apply the workflow in the operating room in patients planned for maxillectomy.

#### **Keywords**

Maxillectomy, 3D VSP, Guided surgery, Zygomatic implants, Prosthetic rehabilitation

## **INTRODUCTION**

Surgical management and oral rehabilitation of patients diagnosed with a maxillary tumour is challenging. The size and extent of the maxillary defect, patient factors, and comorbidities are decisive factors for the choice of surgical, prosthodontic, or combined rehabilitation after a maxillectomy $1.2$ . Different treatment modalities have been described in the literature. Primary closure, prosthodontic rehabilitation by an obturator prothesis, or surgical rehabilitation by tissue grafting the maxillary defect, can be considered in order to obtain the best functional outcome for the patient<sup>3</sup>.

While the functional results of prosthodontic and surgical rehabilitation of smallto medium-sized maxillary defects are somewhat comparable, reconstruction with free flaps seem to provide better speech and swallowing results for extensive or anterior located defects than conventional prosthetic obturation<sup>4</sup>. Supporting the obturator prostheses with implants improves the results of oral function rehabilitation significantly, as well as being a viable technique to improve the functionality of prosthetic rehabilitation in patients who have undergone a maxillectomy<sup>5</sup>. If conventional (obturator) prostheses are expected to be unsuccessful due to, e.g., lack of retention or load bearing problems of the (irradiated) soft tissues, implant placement to support the prosthesis should be pursued.

Unfortunately, implant survival in irradiated maxillary residual native bone seems less predictable in comparison to placement in the mandible<sup>6</sup> (maxilla or mandible, 59% and 85%, respectively;  $p = 0.001$ ). Remote anchorage in zygomatic bone appears to result in higher survival rates. The anchorage in higher level zygomatic bone, subject to lower or no radiation doses, seems favourable when the maxilla is exposed to post-operative radiotherapy<sup>7,8</sup>. An advantage of the use of zygomatic implants after a maxillectomy is the possibility to obtain immediate prosthetic support. Many studies have reported that immediate prosthodontic rehabilitation after ablative surgery is of benefit for the patient7-9. Immediate loading of zygomatic implants is achievable due to a good primary stability in the bicortical plate of the zygoma complex $10,11$ . However, accurate free-hand placement of zygomatic implants, taking the preferred prosthodontic positioning into account, is considered difficult. In the absence of guiding anatomic references, it is challenging to place two zygomatic implants at the defect side because of the long drill path.

With the availability of three-dimensional (3D) techniques, head and neck surgeryguided resections and implant placements, based on a preoperative virtual surgical plan (VSP), is becoming a standard of care<sup>12</sup>. 3D VSP enables a combination of ablation and reconstruction due to the knowledge of the pre-operative size of the defect. This permits 3D planned reconstructions with bone-containing free flaps and ideal prosthetic-driven placement of implants in one surgical procedure<sup>12</sup>. For ablative surgery combined with zygomatic implant placement and prosthetic rehabilitation, 3D virtual planning and computer-aided design have not yet been fully explored.

Although the production of 3D designed implant drill guides is now readily available, the shape and format of zygomatic implants demand a new guide design. The need for a prosthetic angulated implant head to obtain prosthetic support and an ideal screw emergence position on the palatal/occlusal surfaces, together with the implant length, as well as the need for multiple implants and, in oncological cases, the lack of supportive structures, make designing a guide challenging. To the best of our knowledge, a full workflow including tumour surgery, placing of zygomatic implants with 3D printed guides is currently not available. There have been no reports of the design, production, and application of personalized combined bone-supported drill and placement guides for zygomatic implants in order to transfer the virtual planning accurately.

The aim of this study was to develop a workflow that allows one procedure for tumour resection and rehabilitation by immediate placement of zygomatic implants in combination with an implant-retained surgical obturator, as a new treatment modality, using virtual surgical planning. This should lead to optimal placement for immediate loading of the obturator prosthesis as an end result. It is hypothesized that after maxillectomy, the introduction of custom drilling and placement guides for zygomatic implants provides accurate translation of a virtual planning allowing a one procedure workflow for immediate implant-retained prosthetic rehabilitation with a pre-planned obturator prosthesis.

## **MATERIALS AND METHODS**

Cone beam CT-datasets of the skulls of five fresh-frozen edentulous cadavers were obtained (Planmeca, ProMax 3D Max, Stockholm, Finland; 576 slices, voxel size 0.3 mm, FOV:  $11 \times 16$  cm). The settings were in accordance with the clinical settings used for implant planning. A 3D model of the zygomatic bone and maxillae was created using ProPlan CMF 3.0 (Materialise, Leuven, Belgium) software.

#### **Virtual surgical planning**

To mimic the clinical problem of a maxillary defect, typical examples of maxillary tumour resection surgeries were planned virtually (Figure 1a, b). 3D VSPs are created that included partial resection of the maxilla, leaving a maxillary defect, based around an assumed tumour volume that would be suitable for obturator prostheses supported by zygoma implants. The defects created in this experiment were classified as low-level Brown Class 2b maxillectomies $^{13}$ .

Based on the 3D VSP, surgical cutting guides were designed and printed to transfer the resection plan to the cadavers. Next, an obturator prosthesis was designed in the software matching the virtually created defect. Pre-existent dentures were not available for any of the cadavers. The maxillary soft tissues were segmented in order to design digital maxillary dentures as base templates for the final obturator prostheses. Implementing the digital obturator prostheses completed the VSP and enabled the digital planning of the prosthetic implant platform positions.

The position of the zygomatic implants was planned backward from the position of the prostheses. The zygomatic implant heads, to support and fixate the prostheses to the zygomatic implants, were placed in the most ideal prosthodontic positions, slightly palatal from the occlusional plane (Figure 1c, d). In a vertical dimension, enough space for a future bar superstructure and acrylic was taken into account (Figure 1e). Horizontally, the spacing between the prosthetic implant platforms was carefully chosen in order to fit a clip retention system and to enhance any necessary cleaning of the implants (Figure 1f). The positioning of the zygomatic implant was planned with the tip of the implant placed in the lateral cortical bone of the zygomatic complex. The assumption was that placing the apical part of the implant in the cortical bone provides optimal primary stability and will cover the bone on the lateral side of the implant. The preferred apical and abutment positions of the zygomatic implants, implant lengths, and obturator prosthesis were designed virtually. Subsequently, patient specific implant drill and placement guides were designed based on the final virtual set-ups (3Matic Medical, Materialise, Leuven, Belgium) (Figure 1g, h). The drilling/placement guides were developed to fit the following bone structures: alveolar ridge, nasal floor, and zygomatic arch. The guides were printed from polyamide, produced according to the ISO 13485 standards for medical devices, at Oceanz (Ede, the Netherlands). The study ultimately resulted in an advanced implant guide design. The addition of centred channels in the drill-guide enables angled cuts and the length of the channels form an integral depth stop for the drill. The insertion of stainless steel (316 L) milled drill sleeves in the channels should minimize deviation of the drill trajectories. The maxillary bonesupported part included an extension to the nasal aperture to verify good positioning of the guide14 and was connected with crosslink arms to the zygomatic bone-supported part. In addition, the guide was supplied with holes for temporary fixation with mini screws.



**Figure 1.** Overview of 3D VSP workflow, including the anterolateral view (upper row) and the matching caudal view (lower row). The 3D VSP starts with planning of the maxillectomy including the design of the cutting guide, with aim is to remove the purple part representing tumour removal (**a, b**). Hereafter the obturator prosthesis position is planned in the defect with the pre-planned screw access holes (**c, d**). The positions of the zygomatic implants are planned backward from this optimal position of the obturator prosthesis (**e, f**). The final step includes the design of the drilling and placement guide of the zygomatic implants (**g, h**)

#### **Surgical procedure**

The cadaver surgery was split into two series to evaluate the findings and, if necessary, to adjust the guides and/ or obturator prosthesis before the second test. The surgery was performed by OMF surgeons involved in the planning process, and the supportive visual documentation of the planned guide position was always present in the operating room. Two cadaver heads were thawed before surgery for the first session, and the other three were thawed later for the next session.

To create the Class IIb maxillary defects, the cutting guides were placed on the denuded bone of the maxilla and the zygoma (Figure 2a). The stability and fit of the bone-supported cutting guide was verified. The left-sided maxillectomies were guided by the surgical templates. The resected specimen, mimicking a tumour resection, was removed, resulting in a Class IIb defect. The cutting guides were removed and subsequently the implant drilling guide was fitted and placed.

The precise alignment to the underlying bone structures was verified. The drill-guide was fixed to the bone on two anatomical locations (zygoma and premaxilla) using 2.0 mm cortical locking screws (KLS Martin, Tuttlingen, Germany) (Figures 2c and 3a). After drilling, the implant beds through the guide, according to the drill sequence for oncological zygomatic implants (Southern implants, South Africa), the metal sleeves were removed (Figure 3b). The guide was designed to direct the angle and depth of the implant placement (Figure 3c). The VSP planned implant lengths were placed and the final prosthetic platform position was checked by the maxillofacial prosthodontist and the guide was removed (Figs. 2b and 3d). The obturator prosthesis was then fitted, which provided the surgical team with a visual check as to whether the emergence of the zygomatic prosthetic platforms was favourable or not, in relation to the pre-planned slots in the obturator prosthesis. The surgical procedure was finalized by fixating the obturator prosthesis. Nonengaging prosthetic cylinders (Southern implants, South Africa) were fixed to the obturator prosthesis with light cured resin to fix the prosthesis firmly on the zygomatic implant abutments (Figure 2d). The obturator prosthesis was checked for balance support on the contralateral side of the residual maxilla. After the surgical procedure, the obturator prostheses were removed and the heads underwent a post-operative cone beam CT scan to analyse implant accuracy.

In preparation for the second cadaver operation session, two alterations were made to the working method. The first alteration was the use of more rigid and solid crosslink arms on the drilling guide, to minimize guide movement due to vibrations during drilling. Secondly, longer mini screws were used to fixate the guides to the bone. The longer 8 mm screws were better for retention in the slightly porous cadaver bone.



**Figure 2.** Overview of the surgical procedure. The working method starts with left-sided maxillectomy guided by the surgical template (**a**). Next, the drill-guide was fixed to the bone on two anatomical locations (zygoma and premaxilla) using 2.0 mm cortical locking screws and two zygomatic implants were guided placed in the planned positions (**b**). Finally, prosthetic cylinders were fixated to the obturator prosthesis with light cured resin to fixate the prosthesis firmly on the zygomatic implant abutments (**d**)



**Figure 3.** Detailed view of the guide design. In grey the body of the 3D printed polyamide guide **(A)**. In red the planned zygomatic implants. In green the metal inserts used during drilling **(B)**. The metal insert is pushed in the guide by the surgeon during surgery. After drilling the trajectory, the metal insert is removed to accommodate the thicker diameter of the implant. The direction as well as the depth of the implant is set by the design and physical dimensions of the guide **(C)**. After insertion of the implants, the guide is removed by first removing the mini screws (purple) and then removing the guide in the opposite direction of the slots in the implant guide (red arrow) **(D)**.

#### **Outcome measures**

The primary outcome of this study was the fit of the prosthetic cylinders connected to the placed zygomatic implants in the preoperative positioned slots of the obturator prostheses. It was noted if the obturator prostheses needed adjusting to fit the cylinders. Both surgical and prosthetic steps were based on one virtual surgical plan and had to tally with the final positions of the prosthetic implant platform above the designed screw access holes in the dental arch of the obturator prosthesis. In all five cadavers, the support for the obturator prostheses had to be on the remaining maxilla and should match the surgical resection. A placement accuracy of within 3 mm of the prosthetic cylinders in the slots were considered to be successful for a prosthesis, resulting in a passive fit.

A secondary outcome measure for 3D planned series was the zygomatic implant placement accuracy. The post-operative CBCT-data were obtained in a similar fashion as for the pre-operative CBCT. The post-operative maxillae were segmented and, the implant positions were matched with the 3D VSP. The post-operative implant positions are determined by two observers. The most distal part of the long axis of the implant was used as the abutment position (Figure 4a), so that the results were not dependent on a rotation along the long axis. The entry and exit positions in the zygomatic bone were defined by the intersection of this long axis with the virtual maxilla.

Two coordinate systems were defined:

- 1. The Implant's Coordinate System (ICoS); the z-axis runs along the long axis of each planned implant.
- 2. The Occlusion Coordinate System (OCoS); congruent with the axial, saggital, and coronal planes, where the axial plane is defined by the occlusion plane of the virtual obturator prostheses.

The planes perpendicular to the z-axis, and running through the planning's abutment point, defined the entry and exit points for the ICoS measurements. The intersections of the implant long-axes with these planes were defined as the corresponding points of the outcome. Then, the distance between the abutment, the entry and exit points, and their corresponding points were defined. Also, the 3D angular deviations between the planning's and the outcome's long axes were determined (Figure 4a– c). Unpaired t-tests were conducted as well as the intraclass correlation (ICC) of the implant reconstruction between the two observers.



**Figure 4.** Overview of the several types of measurements and reference planes or coordinate systems for assessing the accuracy of zygomatic implant placement derived from post-op CBCT. In red the planned zygomatic implant position, in blue the postoperative zygomatic implant position. **Left:** the implant coordinate system (ICoS) including the three reproducible reference planes in which the accuracy is measured; the centre of the zygomatic implant head, bone entry point of the implant and bone exit point of the implant. Middle: 3D angular deviation between 3D planned position and postoperative implant position. **Right:** Occlusion plane coordinate system (OCoS). A plane parallel to the prosthetic occlusion plane is defined, perpendicular to this plane is the blue arrow. This arrow indicates the direction in which the abutment height accuracy is calculated.

## **RESULTS**

A total of 10 zygomatic implants were placed in 5 cadaver heads. Some minor alterations were made to the guides between the first and second session. Rigidity was improved by increasing the diameter of the crosslink arms and a window was added to the guide to give the surgeon a direct view of the entry point of the zygoma bone. This enabled minimal movement of the guides due to vibration during drilling. Also, longer cortical osteosynthesis screws were used in the second series for guide fixation to the bone. The longer 8 mm screws allowed better retention in the slightly porous bone. Other than this, the planning and guide design was not essentially changed.

## **Outcome measure 1: position of the prosthetic implant platform in relation to the obturator screw access hole**

Non-engaging prosthetic cylinders were screwed in place and the alignment with the screw access holes was checked. All five obturator prostheses could be placed with high accuracy. The outcome in the horizontal as well as in the vertical dimension was within the 3 mm leeway space for the prostheses. The fit of the pre-planned obturator prosthesis was adequate and well balanced on the remaining maxillary structures in all cases. The prosthetic cylinders were integrated into the obturator prostheses successfully in all cases, without needing any further prosthetic adjustments.

#### **Outcome measure 2: implant placement accuracy**

With the aid of the VSP, the drill and placement guides, a total of 10 zygomatic implants were placed. The implant lengths varied between 45 mm and 55 mm and where placed with a mean entry point deviation of  $1.20 \pm 0.61$  mm and a 3D angle deviation of 2.97  $\pm$  1.43° (range 1.0–5.5°). The 3D accuracy of the abutment positions was 1.19  $\pm$ 1.31 mm. The accuracy of the abutment position in the occlusional plane was 1.77  $\pm$ 1.31 mm, with a height accuracy of 1.03 ± 0.85 mm. The complete accuracy results can be seen in Tables 1 and 2. The intraclass correlations (ICC) between the first and second observer for the positions of the abutment, entry-point, exit-point, and 3D angle were 0.91 mm, 1.00 mm, 0.97 mm, and 0.98°, respectively.

No statistical significant differences were found between the mean values of the ventral and dorsal implants ( $P > 0.05$ ). No statistical differences were found between implants placed in the first session and in the second session.

**Table 1.** Accuracy data. Result of the post-op analysis of the implant coordinate system (ICoS) measurements.



**Table 2.** Accuracy data. Result of the post-op analysis. Descriptive statistics of the occlusion coordinate system (OCoS) measurements.



## **DISCUSSION**

This study shows that it is possible to accurately apply 3D virtual planning to guided surgery and implant-retained maxillary prosthetic rehabilitation in one procedure. The described treatment protocol merges 3D virtual surgical planning and 3D virtual prosthetic planning into a single overall treatment modality. Full 3D prosthetic planning offers insight into a maxillary defect size, ahead of ablative surgery, and enables highly accurate prosthetic-driven implant planning as well. Primary implant placement at the time of ablative surgery has been shown to be an effective means of accelerating rehabilitation, along with early loading protocols $5,7,15$ . Placement of implants in one procedure with ablative surgery is an advantage, especially when the oncology treatment requires post-operative radiotherapy for disease control because it avoids the issue of secondary surgery in irradiated tissues<sup>5,7,10,16</sup>. The use of virtual planning techniques to enable accurate guided placement of endosseous implants is now a common procedure, and 3D-assisted planning to determine the ideal zygomatic implant position is used regularly. Some case reports mention surgical navigation as a viable technique to transfer planned implant positions<sup>11,17,18</sup>. However, zygomatic implant placement is challenging because of the long drill path and complex anatomic components. The main drawback of current visualization techniques is the difficulty of maintaining the drilling handpiece steady in the right direction, and transferring the surgical view from the navigation display to the operative site<sup>17,18</sup>. A more reliable transferring method for planned zygomatic implant positions seems to be 3D printed drilling/placement templates. This study demonstrates that it is possible to design one zygomatic drilling template to provide an accurate means of translating the virtual 3D plan. It has been reported that immediate loading of zygomatic implants is a viable treatment option. Boyes-Varley et al.<sup>10</sup> described a workflow where the prosthesis was placed immediately after implant placement in close contact with the implants, but not screw-fixed on the prosthetic implant heads. The prosthesis was resting on top of the zygomatic implants and the obturator prosthesis was fixated to the palatal bone with cortical-osteosynthesis screws. In this study, the obturator prosthesis could be fixated rigidly to the implants without the need for any other fixation, due to the accurate 3D planning of the screw holes in the obturator.

The use of an implant-retained surgical obturator may have a positive effect on the primary stability of the zygomatic implants during bone healing. The obturator prostheses used in this study functioned as an external rigid fixation device that splints the implants together. Primary implant stability is provided just with the zygomatic anchorage, while the coronal fixation is provided by the implant fixated obturator prosthesis. Although the obtained stable prosthetic situation is believed to be effective for some months, eventually it is recommended to pursue cross arch splinting of the zygomatic implants in final prosthetics to contribute to implant survival.

It is reasonable to assume that knowledge of the planned resection automatically provides 3D visualization of the necessary obturator outline to restore oral function. In this study, a treatment protocol is described for immediate prosthetic rehabilitation with immediate loading of the zygomatic implants. Restoring oral function immediately after ablative surgery, in one procedure with implant placement, obviates the need for fitting, placing, and adapting the prostheses. After maxillectomy, the frequent necessity of adjuvant radiotherapy limits the possibility of achieving sufficient retention for a conventional obturator prosthesis. An implant-retained obturator prosthesis allows for repeated removal to check the oncological defect visually, or in the event of complications. The addition of subsequently placing a fixed-removable obturator prosthesis during surgery is a major step to shortening the time of prosthetic delivery and implant utilization. It can be anticipated that the number of prosthetic interventions postoperatively will be less compared to conventional prosthetic planning in which retention is more difficult to obtain. We assume that such patients can recover earlier and better before the often necessary radiotherapy starts and the hospital visits for prosthetic aftercare will be minimized in early postoperative phase.

## **CONCLUSIONS**

This report has introduced a full 3D virtual workflow to enable immediate implant retained prosthetic rehabilitation after a maxillectomy. Zygomatic implants should be placed very accurately in the planned positions using the novel designed patient specific drilling and placement guides, allowing screw-retained fixation of an obturator prosthesis. This concept will be verified next in patients with maxillary cancer who have been planned for prosthetic rehabilitation with an obturator prosthesis.

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# **CHAPTER**

## **Three-dimensional guided zygomatic implant placement after maxillectomy**

4

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*This chapter is an edited version of the manuscript: Three-dimensional guided zygomatic implant placement after maxillectomy.*

Journal of Personalized Medicine 2022; 6;12(4):588.

## **ABSTRACT**

Zygomatic implants are used in patients with maxillary defects to improve the retention and stability of obturator prostheses, thereby securing good oral function. Prosthetic-driven placement of zygomatic implants is even difficult for experienced surgeons, and with a free-hand approach, deviation from the preplanned implant positions is inevitable, thereby impeding immediate implant-retained obturation. A novel, digitalized workflow of surgical planning was used in 10 patients. Maxillectomy was performed with 3D-printed cutting, and drill guides were used for subsequent placement of zygomatic implants with immediate placement of implant-retained obturator prosthesis. The outcome parameters were the accuracy of implant positioning and the prosthetic fit of the obturator prosthesis in this one-stage procedure. Zygomatic implants ( $n = 28$ ) were placed with good accuracy (mean deviation 1.73  $\pm$  0.57 mm and  $2.97 \pm 1.38^{\circ}$  3D angle deviation), and in all cases, the obturator prosthesis fitted as preoperatively planned. The 3D accuracy of the abutment positions was  $1.58 \pm 1.66$  mm. The accuracy of the abutment position in the occlusal plane was  $2.21 \pm 1.33$  mm, with a height accuracy of  $1.32 \pm 1.57$  mm. This feasibility study shows that the application of these novel designed 3D-printed surgical guides results in predictable zygomatic implant placement and provides the possibility of immediate prosthetic rehabilitation in head and neck oncology patients after maxillectomy.

#### **Keywords**

3D; 3D VSP; digital; guided surgery; head and neck oncology; maxillary reconstruction; maxillary tumour; maxillectomy; prosthetic rehabilitation; zygomatic implants

## **INTRODUCTION**

Several reconstructive techniques are available for patients with complex defects of the mid-face and maxilla following tumour resection. The size and extent of the maxillary defect, patient factors, and comorbidities are decisive factors for the choice of surgical, prosthodontic, or combined rehabilitation after a maxillectomy. In cases when tumour resection has caused a relatively small maxillary defect, primary closure or surgical reconstruction with a local soft tissue flap alone can lead to excellent functional and aesthetic results. For larger maxillary defects, reconstruction with a vascularized flap or prosthetic rehabilitation with an obturator prosthesis can be used, the latter remaining an important treatment in many institutions<sup>1</sup>. However, conventional obturator prostheses can have their drawbacks, mainly caused by lack of retention of the prostheses. Placement of endosseous implants in the native bone of the maxilla allow for improvement of retention of the obturator prosthesis and thereby increase the success of prosthetic rehabilitation. While there is often not enough bone volume for reliable implant placement, zygomatic implants can be used to improve the retention of the obturator prosthesis $1=3$ .

The literature reports good zygomatic implant survival rates (78.6 to 100%) after placing maxillary resections<sup>4</sup>. Primary implant placement at the time of ablative surgery along with early loading of implants has been shown to be an effective rehabilitation protocol<sup>1-3</sup>. Although the survival rates are promising, this more complex treatment modality is not a standard implant procedure among many clinicians. Due to drilling with long drills close to critical anatomical structures, compromised visibility, and for oncological cases, also the absence of anatomical landmarks, the oblique drill trajectories for placement of zygomatic implants are challenging<sup>5</sup>. Inaccurate placement could result in uncontrolled bleeding, damage to the orbit and its content, damage to the maxillary sinus, and traumatic fractures to the orbitozygomatic complex<sup>6,7</sup>. Moreover, inaccurate placement and angulation of the implant results in positional errors at the apex and of the prosthetic head. This possibly results in an undesired prosthetic outcome and may even make the use of the zygomatic implant unattainable.

Pre-operative 3D planning and guided placement and drilling according to a virtual surgical plan could solve these problems and result in lower risk of complications compared to the free-hand approach. With the use of virtual implant planning, an optimal inclination, position, and depth of the zygomatic implant can be chosen considering volume and anatomical variation of the malar bone<sup>8</sup>. Moreover, the ideal prosthetic platform positions can be planned, which eliminates the possible need for the intraoperative "guess work" involved with complex zygomatic implant rehabilitation<sup>9</sup>.

While there is widespread experience in guided placement of endosseous dental implants and guided resection of tumours, a proper tool for guided placement of zygomatic implants in maxillectomy patients is not yet available. With the combination of the oblique bone surface, the long drill trajectories and the extent of the defects make designing guided templates a challenge. Any small angular or positional entrance error results in magnification of apical positional error at the tip of the drill<sup>10</sup>. The drill guide for zygomatic implant placement, introduced by Vrielink et al. in 2003, which was solely based on available bone volume, unfortunately had an unfavorable accuracy<sup>11</sup>. A technical note describing guided placement of zygomatic implants in atrophic maxillae lacks implant placement-accuracy analysis<sup>12</sup>.

Recently, our group described a novel design of a fully digital 3D surgical planning for accurately executing the ablative surgery, placement of zygomatic implants, and immediate placement of an implant-retained obturator prosthesis in human cadavers $^{13}$ . Therefore, the aim of this study was to assess whether this full 3D virtual workflow to guiding zygomatic implants placement and providing the patient with a printed surgical obturator prosthesis in head and neck cancer patients with a maxillary defect would be clinically feasible.

## **MATERIALS AND METHODS**

A total of 10 consecutive patients (7 female, 3 male, mean age of 66.3 years, range 45–73 years) who were treated for oral malignancies at the department of Oral and Maxillofacial Surgery at the University Medical Center Groningen were included. Patients either had a pre-existing defect of the maxilla ( $n = 3$ ) or were scheduled for a maxillectomy ( $n = 7$ ) with reconstruction an obturator prosthesis supported by zygomatic implants. All maxillary defects in this study are categorized as a class Brown IIb defect<sup>14</sup>. Patient, tumour, and defect characteristics are described in Table 1. For all patients, a complete 3D virtual surgical planning was made, in which zygomatic implants as well as an implant-retained obturator prosthesis were included.





#### **Pre-Implant Procedure and 3D Planning**

Prior to ablative oncological surgery, each patient underwent a diagnostic work-up consisting of both a CT and MRI of the head and neck region for ablative surgery and implant planning. In dentate patients, the natural dentition of dentulous patients was digitalized through 3D optical surface scanning and could be matched to the 3D patient models. In edentulous cases, additional cone-beam-computed tomography scan (CBCT) datasets of the patients wearing their conventional prostheses were obtained. The patient's prosthesis was prepared before scanning: five radiopaque markers were added and spread over the prosthesis. Immediately after the scanning, a second scan of the prosthesis itself was performed. Through the radiopaque markers, the two CBCTdatasets of the patient and the prosthesis were merged to match the virtual prosthesis to the 3D models of the patient's anatomy.

By using a multi-modality CT and MRI combined workflow for 3D resection margin planning<sup>15</sup>, the tumour was delineated on the MRI data, after which this dataset was fused with the CT bone data in order to construct a 3D bone and tumour model. This model enabled reliable virtual resection planning with oncologic margins16. The virtual patient dentition or prosthesis was matched to the virtual planning to allow for digital obturator prosthesis designing, matching the defect, and backwards planning of the zygomatic implants from the position of the obturator prosthesis. The zygomatic implant heads were placed in the most ideal prosthodontic positions. The apical part of the zygomatic implant was planned in the lateral cortical bone of the zygomatic complex with care for maximal bony contact of the implant. The needed length of zygomatic implant was determined. In dentate cases, two zygomatic implants were digitally planned at the maxillary defect site. Four zygomatic implants were planned in edentulous cases.

### **Guide Design**

Translation of the 3D VSP towards the surgical procedure was realized by means of 3D-printed surgical guides (Figure 1). Subsequently, patient-specific implant drill guides were designed based on the preferred apical and abutment positions of the zygomatic implants captured in the final virtual set-ups (3-Matic Medical, Materialise, Leuven, Belgium). In edentulous cases, the drill guides were developed to fit the alveolar ridge, nasal aperture, and zygomatic arch for stable positioning (Figure 2A,B). The maxillary bone-supported part included an extension to the nasal aperture to verify correct positioning of the guideand was connected with crosslink arms to the zygomatic bonesupported part<sup>17</sup>. Centered channels in the drill-guides enable insertion of stainless steel milled drill sleeves, which should minimize deviation of the drill trajectories and prevent polyamide particle formation (Figure 2C,D). The length of the channels functions as an integral depth stop for the zygomatic implants (Figure 2E,F). In addition, the guide was supplied with holes for temporary fixation with mini screws. If natural dentition was remaining after resection, the teeth were used for support of the guides (Figure 3). The guides were printed from polyamide, produced according to the ISO 13485 standards for medical devices, by Oceanz (Ede, The Netherlands).



Figure 1. Overview of 3D VSP workflow for virtual resection planning. The working method starts with right-sided maxillectomy. **A**, caudal view and **B**, the matching lateral view guided by the surgical cutting guides **C** & **D**, with which the aim is to remove the red transparent part representing tumour removal with margin.



**Figure 2**. Overview of 3D VSP workflow for virtual zygomatic implant planning. **A**,**B** virtual obturator prosthesis driven zygomatic implant planning in an edentulous patient with right sided maxillary resection planning. **C**,**D** bone supported zygomatic implant drill guide. Support is gained at alveolar ridge, nasal aperture and zygomatic arch for stable positioning and centered channels in the drillguide enables insertion of stainless steel milled drill sleeves. **E**,**F** the length of the channels forms an integral depth stop for the zygomatic implants. **G**, detailed view of drill guidance. **H**, detailed view of zygomatic implants placed through the guide to enhance correct prosthetic head positions.



**Figure 3**. Surgical procedure. **A** & **B**, maxillectomy according to the preplanned, individually-designed cutting guides. **C**, drill guide seated with a tight fit and fixated with osteosynthesis screws. **D**, zygomatic drill inserted in the guide to perform the preplanned drill. **E**, insertion of zygomatic implant into the bone until the fixture mount contact the reference stop on the guide. **F**, view of zygomatic implant positions after removing the guide. **G**, final screw direction of the fixture mounts which correspond exactly with the abutment positions. **H**, implant retained obturator prosthesis immediate fixated with non-engaging prosthetic cylinders mounted into the prepared slots with a light curing denture resin.

#### **Surgical Procedure**

First, the tumour was removed by resecting the maxilla (SV) according to the preplanned, individually designed cutting guides (Figure 3A,B). In the two cases in which the maxillectomy already had been performed, a mucoperiosteal flap was raised. Second, the zygomatic implant drill guide was fitted onto the bone. All zygomatic implants were placed by the same surgeons (S.V. and G.R.). During exposure of the maxillary and zygomatic bone, care was taken in order to remove all connective tissue from the guide supporting bone region so that the drill guide could be seated with a tight fit. The guide was fixated with osteosynthesis screws (KLS Martin, Tuttlingen, Germany) (Figure 3C). Third, the first metal sleeves matching the 2.7 mm zygomatic drill with apical lance were inserted in the guide to create the entry point in the malar bone. Subsequently, the preplanned drill trajectories were performed (Figure 3D). The metal sleeve was removed, which transformed the guide into a placing guide for the correct installation angle for the zygomatic implants (Zygex, Southern implants, Gauteng, South Africa). Next, the implants were inserted into the zygomatic bone until the fixture mounts contacted the reference stop on the guide. (Figure 3E). Due to longitudinal slots in the guide, the guide can be removed easily following implant placement by loosening the osteosynthesis screws and unclipping the guide from the implants (Figure 3F). Before removing the guide, the maxillofacial prosthodontist determines the final screw direction of the fixture mount, which corresponds exactly with the abutment position (Figure 3G). The obturator prosthesis with preplanned slots can be used as a reference to ensure a parallel positioning of the prosthetic platforms. In the edentulous cases (n = 5), a second guide was placed on the contralateral side, and the guided implant procedure was repeated. The surgical procedure was finalized by fixating the obturator prosthesis. Non-engaging prosthetic cylinders (Southern implants, Irene) were fixed to the obturator prosthesis with ultraviolet light-curing resin. The obturator prosthesis was checked for balance support and was firmly screw-fixed on the zygomatic implant abutments (Figure 3H). The screw-retained retention allows post-operative removal of the surgical obturator prosthesis and enables replacement as often as necessary.

#### **Analysis of Accuracy**

All patients underwent a routine postoperative cone-beam-computed tomography scan (CBCT) within 16 days after surgery, which was used to evaluate the accuracy of the implant placement. The computer-aided design (CAD) files in STL format of the titanium zygomatic implants were superimposed onto the postoperative CT data, and a comparison was made with the planned positions by calculating reproducible reference planes in which the accuracy was measured. The implant coordinate system (ICoS) includes three reproducible reference planes in which the accuracy was measured: the center of the zygomatic implant head, bone entry point of the implant, and bone exit point of the implant (Figure 4A). Furthermore, the 3D angular deviation between 3D-planned position and postoperative implant position was calculated (Figure 4B).



**Figure 4**. Overview of the different types of measurements and reference planes or coordinate systems for assessing the accuracy of zygomatic implant placement derived from post-op CBCT. In red the planned zygomatic implant position, in blue the postoperative zygomatic implant position. **A**, the implant coordinate system (ICoS) including the three reproducible reference planes in which the accuracy is measured; the centre of the zygomatic implant head, bone entry point of the implant, and bone exit point of the implant. **B**, 3D angular deviation between 3D planned position and postoperative implant position. **C**, Occlusion plane coordinate system. A plane parallel to the prosthetic occlusional plane is defined, perpendicular to this plane is the blue arrow. This arrow indicates the direction in which the abutment height accuracy is calculated. Deviation of the abutment is measured in the occlusional plane (green arrow).

Deviation of abutment position in two dimensions were calculated by defining a plane parallel to the prosthetic occlusional plane as reference: the occlusion plane coordinate system (Figure 4C). If the implant-retained obturator prosthesis on the zygomatic implant abutments was within 3 mm of the prosthetic cylinders in the slots, and a passive fit could be achieved, placement was deemed a success.

## **RESULTS**

#### **Implant Placement Accuracy**

The surgical guides fitted well in 9 cases (28 zygomatic implants). In one case, the fit of the surgical guide was not optimal because a larger resection of the tumour than planned was performed. These two implants were placed non-guided and therefore eliminated from the accuracy analysis. The implant lengths varied between 35 mm and 55 mm and were placed with a mean entry point deviation of  $1.73 \pm 0.57$  mm and a 3D angle deviation of 2.97  $\pm$  1.38° (range 0.6–6.1°). The 3D accuracy of the abutment positions was  $1.58 \pm 1.66$  mm. The accuracy of the abutment position in the occlusal plane was 2.21  $\pm$  1.33 mm, with a height accuracy of 1.32  $\pm$  1.57 mm. An overview of the accuracy results can be seen in Table 2 and Table 3. The accuracy was well within tolerance limits.

**Table 2.** Accuracy data. Result of the post-op analysis of the implant coordinate system (ICoS) measurements and descriptive statistics of the occlusion coordinate system (OCoS) measurements. \* SD, standard deviation.



**Table 3.** Accuracy data. Result of the post-operative analysis. Descriptive statistics of the occlusion coordinate system (OCoS) measurements. \* SD, standard deviation.



## **Fit of the implant retained obturator prosthesis**

In nine cases, the obturator prostheses could be fixated with non-engaging prosthetic cylinders (Zygex Southern implants, Gauteng, South Africa) to the zygomatic implants as planned. The prosthetic outcome in the horizontal and vertical dimension was within the 3 mm leeway space. This margin was available in prepared slots of the obturator prostheses needed for fixation. In the case where the zygomatic implants were not guided placed, extensive prosthetic adjustments at the preplanned slots were needed to allow for a proper fit of the obturator prosthesis. Finally, all pre-operatively designed obturator prostheses had an adequate and were well-balanced on the zygomatic implants and remaining maxillary structures.

## **DISCUSSION**

This feasibility study shows that the application of 3D-printed surgical guides results are feasible in predictable zygomatic implant placement and immediate prosthetic rehabilitation in head and neck oncology patients after maxillectomy. Furthermore, application of this reliable method is believed to minimalize the risk of surgical and prosthetic complications.
The literature reports loading of zygomatic implants within a few hours after implant placement18,19, but to the best of our knowledge, such a CAD workflow involving immediate implant-retained prosthetic rehabilitation in a combined surgical procedure with guided tumour resection and placement of zygomatic implants is not described. Thereby, comparative accuracy data are not available yet. Perioperative prosthetic delivery obviates invasive impression taking in surgical field or shortly after surgery, which is a direct benefit for the patient.

In the literature, an unfavorable zygomatic implant position of the apex or prosthetic head is described as a surgical complication<sup>2,7</sup>. This could indicate that even when executed by experienced surgeons, there is a frequent occurrence of suboptimal zygomatic implant positioning using a free-hand placement. The concept of guided zygomatic implant placement was first tested by our group in a series of human cadavers<sup>12</sup>. The data of this pre-clinical cadaver study and the data presented here are comparable in accuracy. As a consequence, immediate implant support was available for the obturator prosthesis.

This phase I trial shows high clinical potential for this approach of 3D-planned placement of zygoma implants. We think that a larger group of patients is required to confirm our first data on the predictability of placement and subsequent immediate loading of the obturator prosthesis. The lessons learned from this trial are that 3D planning can be accurately used when surgeons and prosthodontists together plan the surgery and prosthetic rehabilitation. 3D visualization of the tumour and planned resection promotes clinical debate and facilitates choices. The execution of the resection is less of a determining factor. Added resections are very well possible since the support for the 3D zygoma guides are chosen outside the expected oncological surgical field. Two factors are critical for accurate placement of the zygomatic implants. The first is the accurate placement of the 3D guide. Surgeons should be aware how the guides should be placed and 3D information should be available in the OR. Time must be taken to place these correctly, as is the case with all 3D-planned surgical guides for another purposes. Second, during placement of the implants, the surgeon should have the possibility of visual inspection of the entry point in the zygoma. Despite accurate 3D planning and well-thought out guide design, the surgeon needs visual feedback on the entry point. Once the entry point is placed accurately, the rigid guide supports the right direction of the implant drill.

Besides guided placement of implants, currently, implant placement using real-time navigation is gaining popularity. Research results are promising, and this most likely accurate and less-invasive surgical technique could be a next step in zygomatic implant placement according to a VSP in the future. To date, the main drawback of current visualization techniques is the difficulty of steadily maintaining the drill handpiece and transferring the surgical view from the navigation display to the operative site, which is amplified in the long drills used for zygomatic implants<sup>20</sup>. Secondly, it currently involves above-average operating time<sup>9</sup>.

It is reasonable to assume that knowledge of the planned resection automatically provides 3D visualization of the necessary obturator outline to restore oral function. In this study, a treatment protocol was used for immediate prosthetic rehabilitation with immediate loading of the zygomatic implants. Restoring oral function immediately after ablative surgery obviates the need for fitting, placing, and adapting the prostheses. After maxillectomy, the frequent necessity of adjuvant radiotherapy limits the possibility of achieving sufficient retention for a conventional obturator prosthesis. An implantretained obturator prosthesis allows for repeated removal to check the oncological defect visually or in the event of complications. The addition of subsequently placing a fixed, removable obturator prosthesis during surgery is a major step to shortening the time of prosthetic delivery and implant utilization. It can be anticipated that the number of prosthetic interventions post-operatively will be less compared to conventional prosthetic planning, in which retention is more difficult to obtain. We anticipate that oral function in such patients can recover earlier and better before the often necessary radiotherapy starts, and the hospital visits for prosthetic aftercare will be minimized in the early post-operative phase. In case of adjuvant radiotherapy, it is important to provide zygomatic implant-specific information to the radiotherapy team. This enables adjustments of the radiotherapy treatment plan and the dosimetric accuracy in radiotherapy $21,22$ .

# **CONCLUSIONS**

A fully digitalized workflow for guided resection, zygomatic implant placement, and immediate prosthetic rehabilitation is feasible when planning a zygomatic implantretained prosthesis. The method presented here is novel and advantageous for head and neck cancer patients because of an immediate implant-based prosthetic rehabilitation after ablative surgery, which otherwise could not have been achieved without delay.

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# **CHAPTER**

**Guided placement of zygomatic implants in head and neck cancer patients: implant survival and patient outcomes at 1–3 years of follow-up**



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*This chapter is an edited version of the manuscript: Guided placement of zygomatic implants in head and neck cancer patients: implant survival and patient outcomes at 1–3 years of follow-up*

International Journal of Oral and Maxillofacial Surgery 2024; 16(4): S0901-5027(24)000572.

# **ABSTRACT**

Zygomatic implants (ZI) are a valuable option for supporting an obturator prosthesis after maxillary resection. This study was performed to assess the clinical outcomes of a digitally validated guided technique for ZI placement, followed by immediate prosthetic obturation. The primary objective was to evaluate implant survival, while the secondary objective was to assess patient-reported quality of life post-rehabilitation. Twelve patients treated for head and neck cancer received a total of 36 ZI after ablative surgery. The mean duration of ZI follow-up was 30.1 months. The survival rate of ZI placed in non-irradiated patients was 100%, while it was 85% in irradiated patients. Patient-reported outcomes were evaluated using the Liverpool Oral Rehabilitation Questionnaire (LORQv3) and the University of Washington Quality of Life Questionnaire (UW-QOL v4). Most patients reported satisfactory outcomes in the oral function domain of the LORQv3 (mean score 17.7 ± 4.5; possible range 12–48, with lower scores indicating better outcomes). Regarding the UW-QOL v4, the swallowing and chewing domains had the highest scores (mean 97.5  $\pm$  8.7 and 95.8  $\pm$  14.4, respectively; maximum possible score of 100). In conclusion, this treatment approach improves function and quality of life after maxillary ablative surgery. However, irradiated patients showed a noticeable trend of higher implant failure, and this was influenced by tumour position and size impacting the radiation dose to the zygomatic bone.

# **INTRODUCTION**

The standard treatment for patients with a maxillary malignancy consists of a (partial) maxillectomy, often in combination with postoperative radiotherapy. The resulting maxillary defect has a profound impact on the patient's functional abilities<sup>1</sup>. The impaired oral functions are often further compromised if post-surgical radiotherapy is needed, due to related radiation-induced sequelae<sup>2</sup>.

The repair of maxillary defects after oncological surgery is possible by means of reconstructive surgery or a prosthetic obturator, depending on patient characteristics, the tumour location, and the surgical team<sup>3</sup>. The overall objective in patients with these maxillary defects is to restore oral function by following a prosthetic-driven reconstruction approach<sup>4</sup>. The choice of reconstruction method in cases of extensive maxillary resection involves a comprehensive evaluation of individual patient factors. While free flap reconstruction remains a robust option for many, the patient's age and health status can influence the decision-making process. Zygomatic implants (ZI) with an obturator prosthesis offer a viable alternative that provides adequate closure of the defect and dental rehabilitation in cases where a less invasive approach is preferred or contraindications for extensive bony reconstruction are present.

In cases where an obturator prosthesis is selected as the primary method of reconstruction, enhancing its retention and stability is crucial. One of the options for improving the retention and stability of obturator prostheses is the application of  $Z^{5}$ . These implants can significantly enhance the functional and aesthetic outcomes for patients while maintaining a patient-centred approach that prioritizes their overall wellbeing and long-term quality of life. The ablation surgery, reconstructive surgery, and prosthetic rehabilitation can be planned preoperatively with the support of threedimensional (3D) virtual surgical planning (VSP) and computer-aided design. The accuracy of this approach has been confirmed in cadaver and feasibility studies<sup>6,7</sup>. The question that still needs to be answered through long-term follow-up is whether this advanced technique results in high implant survival and satisfactory patient outcomes in the long term. Therefore, the aim of this study was to assess the ZI survival rate overall and according to post-surgical radiotherapy data, as well as to determine the patients' self-reported quality of life at 1–3 years after the treatment.

# **METHODS**

# **Study design and patients**

The study was designed as an ongoing follow-up study for monitoring ZI survival and patient outcomes over the long term. All included patients who were treated for oral malignancies,underwent guided maxillectomy followed by reconstruction with an obturator prosthesis, which was supported by immediately placed ZI. The treatment protocol utilizes a novel full 3D workflow. This paper reports the initial phase of the study, at 1–3 years of follow-up after the single-stage treatment procedure.

A VSP was developed for ZI placement and restoration with a screw-retained immediate obturator prosthesis. Before surgery, the patients underwent diagnostic imaging for surgical planning (computed tomography (CT) and magnetic resonance imaging (MRI)). Dentulous patients had their teeth digitally scanned and matched to 3D models, while edentulous patients had additional cone beam computed tomography (CBCT) scans with radiopaque markers on their prostheses. In the constructed 3D models, the ZI were virtually planned based on the occlusion and prosthetic considerations.

The zygomatic oncology implants (Zygex; Southern Implants, Irene, South Africa) were placed by one of two surgeons (G.R. or S.V.). Immediately after guided maxillary resection, the ZI guide was accurately positioned and stabilized, and guided drilling was performed following the manufacturer's recommended drill sequence (Southern Implants protocol). The zygomatic oncology implants were all placed as pairs in the zygomatic bone. Both ZI were placed through the guide into the preferred prosthodontic positions determined before the surgery. Good primary stability was achieved for all of the ZI at the time of insertion. Subsequently, the obturator prosthesis was fitted and the temporary polyether ether ketone (PEEK) abutments were bonded with ultraviolet light curing resin. This enabled stability and retention of the obturator prosthesis and provided the necessary maxillary obturation directly after surgery.

This guided procedure has been described in detail in previous studies<sup>6,7</sup>. All 10 patients from the feasibility study<sup>7</sup> were included in this follow-up study. Following the completion of the feasibility study, two additional patients were treated using this technique and subsequently included in this study. The patients were assessed in the Department of Oral and Maxillofacial Surgery of the University Medical Centre Groningen, the Netherlands. The study was approved by the Medical Ethics Review Board of the University Medical Center Groningen following the guidelines of the Declaration of Helsinki (WMO 202000569).

# **Assessments**

The primary outcome measure was ZI survival. As part of the standard oncological follow-up protocol of the Dutch Cooperative Head and Neck Group, overall disease control is monitored every 3 months. As part of this protocol, a multidisciplinary consultation that included a maxillofacial prosthodontist was conducted to provide the necessary prosthodontic aftercare. All of the patients were monitored closely and had been checked by the maxillofacial prosthodontist (N.V.) within the 3 months prior to the study cut-off date of April 28, 2023.

A CBCT scan was performed and a panoramic radiograph of the implants was obtained directly after surgery. Further panoramic radiographs were obtained after installation of the definitive obturator prosthesis and at 1 year after prosthetic delivery. Regarding the patients who needed postoperative irradiation, the radiotherapy contouring, 3D treatment planning, fractionation, and total dose were reviewed retrospectively. The zygomatic bones of the patients were marked on the CT scan images with specific lines to precisely delineate their size, shape, and location. The implant bed was subsequently verified by imaging until an exact match was found. In this way, accurate radiation doses, including the maximum dose within the ZI implant bed, could be calculated for all of the patients who underwent postoperative radiotherapy.

Patient-reported quality of life after rehabilitation was assessed by administering two questionnaires 4 weeks after the definitive implant-supported obturator prosthesis was placed. In the first questionnaire, the Liverpool Oral Rehabilitation Questionnaire (LORQv3; Dutch version), of the total questionnaire, 27 questions can be divided into four domains consisting of (A) oral function, (B) orofacial appearance, (C) social interaction, and (D) patient/prosthetic satisfaction. The items are rated on a 1–4 Likert scale, with  $1$  = never,  $2$  = sometimes,  $3$  = often, and  $4$  = always; lower scores indicate better outcomes.

The second questionnaire, the University of Washington Quality of Life Questionnaire version 4 (UW-QOL v4)<sup>8</sup>, is a widely used tool for the evaluation of health-related quality of life in patients with head and neck cancer<sup>9</sup>. It consists of 12 questions concerning pain, appearance, activity, recreation, swallowing, chewing, speech, shoulder function, taste, saliva, mood, and anxiety domains. The answers to each question are scored from 0 to 100, with 100 being the best score.

# **Statistical analysis**

The statistical analysis was restricted to descriptive statistics, which were calculated using IBM SPSS Statistics version 28.0.1.0 (IBM Corp., Armonk, NY, USA).

# **RESULTS**

At the data cut-off point (April 28, 2023), 12 patients (seven female, five male), with a median age of 66 years (range 45–87 years), had undergone the procedure and had been followed-up for a minimum of 1 year post-rehabilitation. The maxillary abnormality diagnoses are summarized in Table 1. In total, 36 guided ZI were placed. Among the 12 patients, eight were edentulous when treatment started, of whom six received four ZI, while two received two ZI on the defect side and endosseous implants (Nobel Parallel; Nobel Biocare, Gothenburg, Sweden) were placed in the contralateral native maxilla. The other four patients were dentulous, they all received two ZI on the defect side. Three of them also received endosseous implants(Nobel parallel, Nobel Biocare, Gothenburg, Sweden) in the shortened contralateral dental arch for further prosthetic retention. All of the patients received a definitive implant-retained obturator prosthesis to replace the fixed surgical obturator prosthesis. Six patients needed postoperative radiation due to the T and N cancer stage. The postoperative radiotherapy dose to the ZI site ranged from 2 Gy to 128 Gy (median dose 40 Gy). An overview of the patient characteristics is shown in Table 2.



**Table 1.** Maxillary abnormality diagnoses (12 patients).

ORN, osteoradionecrosis.

### **Table 2.** Patient characteristics.



RT, radiotherapy; SD, standard deviation.

# **Implant survival**

At the data cut-off point, the overall ZI survival rate was 91.7%, with a 100% survival rate in the non-irradiated group of patients and 85% survival rate in the irradiated patient group; the mean  $\pm$  standard deviation implant follow-up period was 30.1  $\pm$ 11.1 months (Table 3).



# **Table 3.** Implant data.

A total of three ZI failed in two irradiated patients: one patient lost one implant and the other patient lost two. One failure was a ZI placed on the dorsal side of the defect, which had received 57.4 Gy post-surgically. Implant mobility was observed during the prosthetic aftercare. The same patient had received a second more ventrally placed ZI during the same surgery. Despite receiving an equal dose of radiotherapy, the implant functioned successfully while loaded with a magnet attachment to achieve prosthetic retention within the defect area. Thus far, no postoperative complications have been observed for this implant. The two other failures were in a patient who received pre- and postoperative radiotherapy. Before the ablative surgery, the zygoma bone was subjected to irradiation, up to a dose of 58 Gy, and unfortunately shortly after surgical treatment a recurrence was observed. An additional dose of 70 Gy was then delivered, bringing the total dose to 128 Gy. The guiding principle is to achieve the desired dose coverage to the target volume while sparing organs at risk (OAR) as much as possible. The dose–volume histograms of both radiotherapy treatment plans were used to evaluate the re-irradiation constraints for the OAR such as the brainstem, spinal cord, larynx, and bone (including the ZI). The boundaries for 'acceptable damage' are therefore different for the re-treatment situation than for the initial treatment, and in this situation maximum doses higher than 100 Gy to the bone are unfortunately not uncommon in head and neck cancer patients, especially when the OAR lies within the target regions $10,11$ .

# **Patient-reported outcomes**

All of the study patients completed the LORQv3 and UW-QOL v4 questionnaires at 4 weeks after the final obturator prosthesis had been placed. An overview of the questions and domains of the LORQv3, and the mean ± standard deviation scores for the 12 patients, are given in Table 4. The domains of the UWQOL v4 and the mean  $\pm$ standard deviation scores for the 12 patients are listed in Table 5



**Table 4.** Liverpool Oral Rehabilitation Questionnaire (LORQv3) scores for the 12 patients with zygomatic oncology implant-supported obturators.



**Table 4.** Liverpool Oral Rehabilitation Questionnaire (LORQv3) scores for the 12 patients with zygomatic oncology implant-supported obturators. *(continued)*

SD, standard deviation.

a Score on a 1–4 Likert scale, ranging from 1 'never' to 4 'always'; lower scores indicate better outcomes.

**Table 5.** Mean scores for the 12 domains of the University of Washington Quality of Life questionnaire (UW-QOL v4), for the 12 patients with zygomatic oncology implant-supported obturators.



SD, standard deviation.

a Score on a scale of 0–100, with higher scores indicating better outcomes.

The mean overall score for section A of the LORQv3, covering oral function, was 17.7  $\pm$ 4.5 (possible range 12–48, with 12 representing the best oral function). This indicates a satisfactory outcome for this domain, and is comparable to the results of other studies<sup>12</sup>.

Regarding the UW-QOL v4, the scores for the 12 domains were normally distributed; the mean values are shown in Table 5. Swallowing and chewing were the best scoring domains, with a mean score of 97.5  $\pm$  8.7 and 95.8  $\pm$  14.4, respectively; 11 out of the 12 patients gave responses for these domains with the best possible score of 100. The worst score was for anxiety, with a mean score of 70  $\pm$  0.0; all 12 patients marked the box "I am anxious about my cancer" (score 70). When selecting the three most important domains, activity was considered by the patients to be the most important.

# **DISCUSSION**

This study showed that ZI placed under guidance and immediately loaded with an obturator prosthesis had a high survival rate after a minimum period of 12 months. The overall implant survival rate of 91.7% is consistent with other studies in which ZI have been used to improve prosthetic management in head and neck cancer patients<sup>13</sup>. Compared to the use of ZI for prosthetic rehabilitation in patients with extreme resorption of the maxilla, with a mean survival rate of 96.5%, the rate in the current study is slightly lower $14$ .

In terms of compromising the soft tissues, the placement of endosseous implants has a less invasive impact when compared to ZI. Endosseous implant placement should be considered when the bone volume in the native maxilla remains sufficient after a maxillectomy. In this study, the residual maxillary bone volume in two of the edentulous patients was good and it was possible to place endosseous implants in the contralateral maxilla instead of ZI. However, the combination of ZI and endosseous implants had drawbacks regarding the time to prosthetic delivery. Compared to the edentulous patients rehabilitated with four ZI, there was a delay of 3 months for installation of the definitive implant-retained obturator prosthesis in these patients. Despite needing additional prosthodontic appointments, as well as interim obturator prostheses, the final prosthetic result was within expectations (Figs. 1 and 2).



**Figure 1. (A)** Panoramic radiograph and **(B)** intraoral views of a patient with a U-shapedcross-arch suprastructure on four zygomatic oncology implants, two positioned in the defect and two on the contralateral side. **(C)** The matching definitive implant-retained obturator prosthesis.





**Figure 2.** (A) Panoramic radiograph and **(B)** intraoral views of a patient with a U-shaped cross-arch suprastructure on two zygomatic oncology implants positioned in the defect and two endosseous implants in the maxilla on the contralateral side. **(C)** The definitive implant-retained obturator prosthesis.

Implant and prosthetic success are not the only outcomes that should be evaluated in terms of treatment success. The importance of patient quality of life after cancer treatment has become more significant over the past decade<sup>15</sup>. Rehabilitation with the definitive implant-retained obturator prosthesis resulted in favourable patientreported outcomes, as shown by the results for the UW-QOL v4. Overall quality of life several months after the treatment was good or very good. Regarding the LORQv3, the worst scores were obtained for the domain 'salivation' and for the question on problems with mouth opening. The patients who reported that they often or always experienced problems with these items had all undergone postoperative radiotherapy. Thus irradiation leads to a higher risk of impaired oral function, specifically in relation to mouth dryness and trismus<sup>16</sup>.

Caution should be taken with implant placement when radiation is part of the treatment plan17. Metallic artefacts, such as in ZI, still pose a major challenge for radiation therapy, as they impact the target volumes, type of radiation, and dose of radiation $18$ . In the case of maxillary tumours, the zygomatic bodies are often subjected to irradiation, which therefore reduces the osseointegration potential. Although several papers have reported significant ZI failure rates of up to  $31\%$  in irradiated patients<sup>19-21</sup>, it appears that the specific radiotherapy dose to the zygomatic bone in maxillary tumour patients has thus far not been specifically analysed or correlated with ZI failure. In this study, the radiation dose for each ZI was visualized. Implant bed-specific dosages differ significantly depending on the location of the primary tumour<sup>22</sup> (Figure 3), and more than 55 Gy seems to be a risk factor for peri-implant bone resorption and ZI loss.



**Figure 3.** Images **A** and **B** show accurate radiotherapy dose distributions **(orange 56 Gy, green 40 Gy, and blue 20 Gy)** for the primary tumour site, zygomatic bone, and zygomatic implants. Comparison of images A and B shows the significant differences in implant bed-specific dosages based on the location of the primary tumour.

The implant survival rates in this study with follow-up of 1–3 years are favourable, and the patients reported favourable functional outcomes, which suggests that this a worthwhile therapeutic solution. Although the integration of the ZI was successful in the irradiated patients, there was a trend of higher ZI implant failure in the group of patients who underwent postoperative radiotherapy.

A limitation of this study is the sample size of head and neck cancer patients who received ZI; this may limit the generalizability of the findings. Long-term, prospective, longitudinal research involving a larger cohort of participants is required. Additionally, there is a need for an increased dataset that includes information on radiotherapy fields in relation to ZI.

The position and size of the tumour have a direct impact on the radiation dose to the zygoma bone. Greater insight into these relationships would contribute to a better understanding of the expected survival rate of zygomatic implants in patients who need adjuvant radiotherapy. Good dialogue and exchange of information between the surgical team and radiation oncologists is important and could contribute to the long-term success of zygomatic implant-based rehabilitation in head and neck cancer patients.

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# CHAPTER 6.1

# **Patient-specific sub-periosteal zygoma implant for prosthetic rehabilitation of large maxillary defects after oncological resection**

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*This chapter is an edited version of the manuscript: Patient-specific sub-periosteal zygoma implant for prosthetic rehabilitation of large maxillary defects after oncological resection* 

> International Journal of Oral and Maxillofacial Surgery 2019; 48(1):115-117.

# **ABSTRACT**

A 74-year-old woman needed a subtotal bilateral maxillectomy due to squamous cell carcinoma of the palate. Immediate and secondary reconstruction of the defect was not feasible, so the defect was closed with an obturator prosthesis wired to the zygoma complex. To improve the patient's severely impaired speech and swallowing, a patientspecific sub-periosteal implant (psSPI) was designed that matched the remnants of the zygoma complex. First, the patient's post-surgical anatomy was visualized through segmentation of the pre- and post-maxillectomy computed tomography data. Next, based on the data, a customized zygoma-supported framework was designed to support the obturator prosthesis. Surgical guides for intraoperative navigation were designed and three-dimensionally printed, along with an obturator prosthesis to fit the planned outcome situation. The preoperatively manufactured psSPI and obturator prosthesis matched the intraoperative conditions. The postoperative results were favourable; within a week after surgery the patient could speak and swallow normally without nasal leakage. No problems occurred during follow-up. These results indicate that a psSPIretained prosthesis can be considered for the restoration of speech and oral functioning in cases with a largely compromised maxillary bone anatomy, accompanied by impaired oral functioning and no feasible conventional reconstruction options.

# **INTRODUCTION**

The rehabilitation of large maxillary defects resulting from ablative tumour surgery is a reconstructive challenge. To restore oral function and preserve psychological wellbeing, reconstruction can be achieved through conventional approaches, such as closure of the maxillary defect by microvascular free flap surgery or prosthetic obturation $1,2$ . In both treatment options, osseointegrated implants can enhance the stability and retention of the prosthesis. Occasionally, zygoma implants cannot provide satisfactory implant anchorage due to insufficient bone volume, but these patients still need an adequate implant-retained obturator prosthesis. Otherwise, oral functions like mastication, swallowing, and speech remain severely impaired. Recently, Mommaerts introduced an innovative concept for an additivemanufactured sub-periosteal jaw implant that uses modern computer-aided design and manufacturing (CAD/CAM) technology<sup>3</sup>. His approach offers an alternative implant option for patients with extreme jaw bone atrophy. He also suggested that this technique could be used for the rehabilitation of extended post-resection defects. However, tissue conditions after oncological resection and postoperative radiotherapy require a specific design due to the lack of sufficient bone to support even a subperiosteal implant.

# **Case presentation**

A 74-year-old female patient was treated with a subtotal bilateral maxillectomy due to squamous cell carcinoma of the palate. Seven years before, the patient had received primary radiotherapy (cumulative dose 60 Gy) for squamous cell carcinoma of the floor of the mouth. To restore speech and swallowing, the resulting maxillary defect was obturated perioperatively with an obturator prosthesis. The obturator was fixed bilaterally with wires around the zygomatic arches. However, the patient developed postoperative swallowing and speech problems due to loosening of the prosthesis. Moreover, the patient experienced increasing problems with cleaning the prosthesis, which resulted in halitosis and a severe negative impact on quality of life. Surgical restoration of the maxillary defect was not feasible due to the patient's poor medical condition, in particular compromised vascularization. As insufficient bone support was present for placement of dental or zygomatic implants to support a prosthesis, a patient-specific sub-periosteal zygoma implant (psSPI) was developed. This psSPI was provided with an implant-supported obturator prosthesis, which was retained to the framework with anchor attachments (the Swiss Dalbo-System) (Figure 1).



**Figure 1.** The additive manufactured patient-specific sub-periosteal implant (psSPI). Rendered three-dimensional model of the patient showing the implant matching the anatomical geometry of the zygoma remnants. Only the extensions of the two connectors on which the U-shaped framework is situated penetrate the oral mucosa, which makes cleaning the psSPI easier. Note the insert showing the additive manufactured psSPI with the implant-retained obturator prosthesis in place.

# **MATERIALS AND METHODS**

# **Design**

Prior to ablative oncological surgery, the patient's functional prosthesis was digitized through three-dimensional (3D) optical surface scanning. This virtual prosthesis model was matched to 3D models of the patient's anatomy – the starting point for the psSPI design. The planned position of the prosthetic dental arch was determinative for the

location of the four anchor attachments. On these attachments, a U-shaped framework was designed to support the obturator prosthesis. After designing the basal structure of the psSPI using CAD techniques, two connectors were designed to fix the psSPI to the zygomatic bone. As part of the design, the preferred screw and retention positions were taken into consideration, thereby circumventing the irradiated areas of the remaining maxillary and zygomatic bone. Only the extensions of the two connectors on which the U-shaped framework was situated penetrated the oral mucosa, making it easier to clean the psSPI. Materialise 3-matic version 11.0 (Materialise, Leuven, Belgium) and SolidWorks Professional 2017 (Dassault Systèmes, SolidWorks Corp., Waltham, MA, USA) software was used to design the psSPI. In addition, a patient-specific surgical drill guide was designed to translate the 3D plan to the surgical procedure. Furthermore, based on the 3D design, a temporary obturator prosthesis with four Dalbo attachments was manufactured prior to the surgical procedure. The psSPI was manufactured by Witec (Witec Fijnmechanische Techniek BV, Ter Apel, the Netherlands) from medicalgrade titanium alloy (Ti–6Al– 4V). Threads matching 2.0-mm locking screws (KLS Martin, Tuttlingen, Germany) were added to the screw holes.

## **Surgical procedure**

Under general anaesthesia, a full-thickness flap was raised to expose the remnants of the zygomatic bone. The stability and fit of the bone-supported surgical template was then verified. Guided by the surgical template, the holes for the locking screws were drilled. To align the implant to the drilled holes, the implant was positioned using stainless steel (316L) pins prior to screw insertion. This approach resulted in precise alignment of the psSPI with the underlying zygomatic bone. The psSPI was fixed with the locking screws. Next, the fit of the obturator prosthesis on the U-shaped part of the psSPI was checked, and the mucoperiosteal flap was repositioned and sutured (Vicryl 3–0; Johnson & Johnson, Brunswick, NJ, USA). Finally, the implant-retained obturator prosthesis was placed by the prosthodontist. Only minor adjustments had to be made to the base of the prosthesis to obtain optimal obturation of the defect.

# **RESULTS**

Recovery from the procedure was uneventful. Obturation of the defect was satisfactory. Within 1 week, speech performance was favourable and there was no nasal leakage during swallowing. Two weeks after surgery, the sutures were removed. Oral inspection showed no signs of inflammation or dehiscent bone, and an uncomplicated adaptation of the soft tissues around the arms of the psSPI was apparent. During the next 6 months (final follow-up), the soft tissue remained in a good condition (Figure 2) and the obturator prosthesis functioned well. The patient felt confident with wearing the prosthesis and was very satisfied. She spontaneously reported recovery of her social life as a major achievement.



**Figure 2.** Clinical view of the patient-specific sub-periosteal implant (psSPI). Intraoral view 6 months after surgery showing the large oronasal defect, the psSPI, and healthy peri-implant tissues.

# **DISCUSSION**

This customized, prosthesis-driven implant design offers an alternative approach for the rehabilitation of large maxillary defects in cases where immediate or delayed surgical reconstruction is not feasible and oral functioning and oral cleaning are impaired. The easily removed obturator prosthesis is a major benefit. This allows examination of the tissues and enables patients to maintain and clean the prosthesis and periimplant tissues themselves. Although sub-periosteal implants have fallen into disuse due to severe inflammation and inappropriate or non-rigid fixation<sup>4</sup>, the design used here enabled us to provide a solution for a patient without other treatment options, resolving her poor oral functioning and impaired oral health-related quality of life. Furthermore, titanium is more tissue-friendly than the chrome–cobalt alloys that were used in the previous sub-periosteal implants. As it had to be determined beforehand whether the psSPI would be able to withstand chewing forces, a finite elements analysis was performed to assess implant strength and fatigue resistance (data not shown). This analysis revealed that the psSPI could easily bear occlusal loading. We therefore recommend the digitally planned psSPI to provide effective support for obturation of large maxillary defects in patients for whom a direct or delayed restoration of the defect is not feasible.

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# CHAPTER 6.2

# **Differences in approach for sub-periosteal zygoma implant designs**

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*This chapter is an edited version of the manuscript: Differences in approach for sub-periosteal zygoma implant designs*

International Journal of Oral and Maxillofacial Surgery 2019; 48(12):1605-1606. We agree that maximal benefit should be taken from existing anatomical structures. However, in oncology cases such as the one we reported, with an extensive maxillary defect due to ablative surgery, there is a lack of such anatomical structures (Figure 1). Moreover, most patients with large maxillary defects have been subjected to postoperative radiotherapy, which further challenges implant placement because of the inherent risk of developing osteoradionecrosis.



**Figure 1.** Orthopantomogram showing extensive maxillary defects due to ablative surgery and lack of anatomical structures to allow vertical support. To deal with the lack of anatomical support and compromised tissues, a finite element analysis was performed to design a slim, minimal voluminous sub-periosteal zygoma implant (psSPI) that can be reliably fixed to the remaining zygomatic bone.

In the case presented, the volume, surface, and amount of permucosal connection of the sub-periosteal zygoma implant design was not only prosthetic driven, but also accounted for the minimal available bone remnants after a high resected maxillectomy and the fragility of the irradiated tissues. To deal with such a lack of anatomical support and compromised tissues, as well as our endeavours towards a slimmer and less voluminous single sub-periosteal zygoma implant (psSPI) design, we performed a finite element analysis (FEA) to ensure stable fixation of the psSPI to the available zygomatic bone. In addition, we applied locking screws to obtain en-bloc stabilization. This FEA approach indicated that no failure of the designed implant will occur within 1.75  $\times$ 107 loading repetitions, reflecting 25 years in vivo<sup>2</sup> . Matching an 18-month follow-up computed tomography (CT) scan to the CT scan obtained directly postoperative revealed a maximum measured deviation of 0.44 mm (Figure 2). This deviation includes errors of both CT scans (0.4 mm and 0.6 mm thickness), segmentations, and superimposition of the models.



**Figure 2.** Segmentations of the patient's skull derived from the direct and 18 months postoperative CT scans were aligned using the Best Fit Alignment tool in Geomagic Studio 5 2012 (3D Systems, Rock Hill, SC, USA) software whilst moving along an identical CAD file of the implant. Note the nearly perfect alignment of direct postoperative (grey) and 18 month follow-up (blue) implant position. This nearly perfect alignment indicates good clinical implant stability.

While Mommaerts used sandblasting, acid-etching, and plasma surface activation for the surface of his implant<sup>3</sup>, we opted for high-gloss, polished, milled titanium in order to ease intraoral cleaning. Moreover, as we used locking screws, we did not need osseointegration-promoting surface modifications. With regard to Mommaert's concerns with not using disconnectable posts, it is our opinion that the use of disconnectable posts would be of no added benefit and would even counteract the slim and less voluminous design we prefer for oncological cases. The latter because caution has to be taken in oncology cases when it comes to penetration of the compromised soft tissues due to scarring and/or radiation injury. Therefore, we made the deliberate decision to minimize the amount of permucosal connection and thereby reduce the risk of peri-implant mucositis developing. Furthermore, the FEA showed that there was no need for additional posts to increase vertical support, which is a great achievement in oncology cases in which the implant is placed in highly irradiated tissues. In the event of peri-implantitis occurring, there is a very high risk of developing osteoradionecrosis. The occurrence of osteoradionecrosis in our patient case would result in loss of the implant, with likely substantial bone loss and a maxillary defect that would be very difficult to treat. To safeguard a good result, we have imposed strict hygiene recall appointments. Professional cleaning of the oral cavity and the implant during the recall visits, in addition to strict oral hygiene maintenance by the patient herself, will be of the utmost importance to prevent signs of inflammation and diagnose these early. Our

patient has reported no discomfort or pain. No signs of the development of peri-implant mucositis or peri-implantitis have been observed by the dentist or oral hygienists during the 18 months of follow-up to date since placement of the psSPI. The additively manufactured sub-periosteal jaw implant – AMSJI – developed by Mommaerts is a valid treatment option for excessive maxillary bone loss, poor bone quality, and maxillary pneumatization<sup>3</sup>. However for oncology cases, such as our case, an unmodified Mommaerts approach is not applicable, as that approach relies on vertical support and fixture on maxillary and palatal bone structures that are often no longer present.

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# **CHAPTER**



#### **GENERAL DISCUSSION**

This thesis demonstrates the need for integrating 3D VSP and computer-aided design (CAD) in complex prosthodontic rehabilitation. In chapter 2, the current challenges and new developments in literature on prosthodontic management of head and neck cancer patients is described. A synergy of various digital workflows regarding treatment and rehabilitation contribute to a better prosthodontic outcome and thereby enhance the well-being and comfort of patients undergoing maxillary resections. By obtaining a three-dimensional understanding of resection planes prior to surgery<sup>1,2</sup>, valuable insights into the expected dimensions of the post-resection defects is gain. This, in turn, enables to digitally design and fabricate a surgical obturator prosthesis (figure 1A-F) before the ablative surgery, ensuring a precise fit with only minimal per-operative adjustments required. In the literature a limited number of case reports and series on this subject is reported $3-6$ . Although studies comparing digital and conventional workflows are still lacking, the utilization of CAD-CAM obturator prostheses has shown promising outcomes in terms of improved prosthetic base and obturator part fit. Additionally, these prostheses, whether printed or milled, offer the advantage of reduced weight due to differences in material characteristics, thereby enhancing the effectiveness and comfort of head and neck cancer patients, especially during postoperative radiotherapy when dealing with radiotherapy-induced mucositis. It should be noted that the 2017 amendment to the Medical Device Regulations (MDR) in the European Union allows in-house 3D printing of custom medical devices like obturators, but strict adherence to guidelines is required<sup>7</sup>. This necessitates expertise in regulatory compliance and thorough documentation of processes. Continuous training is essential to stay updated on regulations. In-house 3D printing offers possibilities, but strict compliance with regulations is vital for patient safety and MDR adherence.



**Figure 1A-F.** Digital workflow for an obturator prosthesis. **A**. osteotomy planes and tumour visualisation. **B-E**. obturator design based on planned maxillary resection. **E**. peroperative view of obturator prosthesis.

Dental implants have shown to be a great asset to support maxillary prosthodontic rehabilitation in head and neck cancer patients<sup>8-10</sup>, particularly in edentulous cases with an extensive maxillary defect involved implant support for prosthetic rehabilitation is desirable. The larger the defect, the more pronounced the benefit of implants is for the patients in terms of treatment outcome. Based on the scoping review on the optimal timing of implant placement in head and neck cancer patients (chapter 2), it was determined that the timing of implant placement had no impact on implant survival rates, regardless of whether they were placed during ablative surgery or after the completion of oncologic surgery. This finding aligns with our institution's standard practice, which favors implant placement during ablative surgery. As a result, the majority of implants are inserted at this stage, providing the advantages of avoiding the need for an additional surgery for the patient and potentially expediting the process of receiving their prosthesis<sup>11</sup>. Secondary placement is only performed under specific circumstances, such as when patients were initially managed elsewhere without implants or when the loss of prior implant(s) compromises the retention of the prosthesis.

While there is often not enough bone volume for reliable implant placement, zygomatic implants can be used to improve the retention of the obturator prosthesis. However, placement of these implants after maxillectomy is challenging and is noted for its risk at implant failure, poor placement or positioning and mucosal complications $12-14$ . The guided zygomatic implant placement technique introduced in this thesis (chapters 3,4 and 5) uses patient specific drill guides to transfer the preplanned implant positions towards the patients. This novel 3D workflow ensures safe and predictable zygomatic implant placement. However, from a prosthodontic standpoint, the transcendental step in the 3D workflow is the ability to safeguard optimal positioning of the implant heads and create a matching 3D-designed and milled obturator prosthesis (figure 2 A-D). The ability to immediately fixate the obturator to the guided placed zygomatic implants in one procedure with ablative surgery is a game changer in terms of immediate prosthodontic rehabilitation and is currently a proven method. Chapter 5 shows for this technique favorable implant survival rates up to three years post-treatment. However, irradiated patients showed a noticeable trend of higher implant failure ( non-radiated patients 100%, while in irradiated patients 85%), influenced by tumour location and size, impacting radiation dose on the zygomatic bone.



**Figure 2A-D. A-C.** prosthetically driven virtual implant planning of zygomatic oncology implants that places the implant heads in a parallel and prosthodontic favorable position. **D**. the matching digital designed obturtor prosthesis.

#### **Multidisciplinary team**

In such combined surgical and prosthodontic 3D workflows, effective multidisciplinary collaboration is essential in order to meet the constraints in lead-time set by Dutch oncological regulations, which determine the timeframe between oncological diagnosis and treatment. 3D virtual prosthodontic planning is the final step of the preoperative planning and manufacturing process of guides. Customized prostheses tailored to the patient's specific virtual maxillary resection can pose challenges in terms of time constraints. It is necessary to thoroughly review and reach a consensus on the oncological surgical planning before initiating the virtual prosthetic planning, followed by the 3D printing of surgical guides and the milling of the prosthesis, all of which must be completed prior to the surgical procedure. While time pressure can be demanding for the team during the preoperative phase, in the long run, the utilization of 3D surgical and prosthodontic planning facilitates a reduction in the overall treatment duration and is believed to minimize the burden on patients compared to analogue prosthodontic rehabilitation techniques. It is to be expected that in the near future virtual techniques can reduce the lead-time of the aids and parts needed. A new wave of advancements like virtual, augmented reality and robotic surgery show promising results in accuracy<sup>15-18</sup>. Therefore, a possible next step towards an accurate surgical outcome might involve replacing printed guides by virtual techniques that allow the omission of physical 3D printed guides regarding the surgical procedure.

The implementation of our digital prosthodontic pathways for maxillary defect rehabilitation represents a significant advancement in head and neck cancer treatment. By leveraging 3D technology and personalized treatment planning, we aim to enhance the quality of life for patients undergoing maxillary resection. However, the patient still relies on the clinical skills of the maxillofacial prosthodontist within the context of modern healthcare. To implement 3D workflows in maxillary prosthetic rehabilitation for head and neck oncology patients, teams must be willing to work multidisciplinary and discuss and plan surgical treatment in alignment with potential prosthetic rehabilitation. The head and neck oncology team in Groningen has the privilege to collaborate with highly experienced technical physician specialists and design specialists from the 3D lab at the UMCG. Optimizing and initiating 3D workflows, and thus the completion of this thesis, could not be accomplished without this collaboration. At present, the ability to directly place implants as a team during oncological surgeries and/or to have a maxillofacial prosthodontist present during the surgical procedure for prosthodontic treatment is not yet implemented in all head and neck oncology centers. There is a general consensus about the importance of accessible innovative medical care for all patients, mandating medical institutions to exchange information and adopt new treatment methods as presented in this thesis. Uniform collaboration with a widely diversified surgical team in other clinics is indispensable to obtain data for further research and clinical studies to assess the long-term outcomes and efficacy of this approach. Consequently, the Department of Oral and Maxillofacial Surgery in Groningen has already initiated courses for guided placement of zygomatic implants for multidisciplinary head and neck cancer teams.

#### **Radiotherapy**

As mentioned earlier, dental implants have the potential to enhance oral function recovery through the use of implant retained fixed or removable prostheses. With the increasing life expectancy of patients, it is crucial to prevent treatment-related harm that can significantly impact the quality of life and daily functioning of head and neck cancer (HNC) patients. The Normal Tissue Complication Probability (NTCP) model is widely employed in radiotherapy to predict the risk of complications in healthy tissues and organs resulting from radiation exposure<sup>19</sup>. This model aids in assessing potential side effects of radiotherapy and allows radiation therapists to plan treatments that optimize the dose to the target area while minimizing damage to surrounding healthy tissue. Organs at Risk (OARs) refers to healthy organs and tissues near the treatment area that are susceptible to radiation-induced damage. In the case of head and neck cancer patients, OARs encompass organs such as the brain, salivary glands, and thyroid glands, which are associated with various toxicities and symptoms including swallowing difficulties, salivary dysfunction, mucosal changes, speech impairments, pain, and general complaints. Although oral function-related complications are considered in the NTCP model, the dental implant site in the bone necessary for restoring oral function are not recognized as OARs. In our care path implant placement during the ablative surgery, aims to ease the prosthodontic rehabilitation after oncological treatment. The loss of dental implants in irradiated patients results significant consequences to wearability of a prosthesis and thereby impacting speech, chewing abilities, pain and significantly compromising quality of life. Placement of implants in second stage surgery after radiotherapy is usually not feasible in this high dose radiated patient group. Therefore, it is recommended to include dental implant sites as prioritized organs for sparing in relation to high-impact symptoms.

#### **Future perspectives**

The successful implementation of 3D workflows in maxillary prosthetic rehabilitation of head and neck oncology patients represents a notable achievement. However, the journey does not end here. Future research should focus on refining these workflows, prioritizing patient-centered care and fostering multidisciplinary collaboration. By doing so, we can continue to improve the quality of life and treatment outcomes for the head and neck cancer patient population.

1. The focus of next phase research in this field should be on resolving the issues of time constraints in the planning of head and neck oncology patients. In the Netherlands guidelines state that patients should be treated within 30 days after the primary visit. Therefore, studies should be initiated assessing whether replacing the printed guides by virtual techniques is an accurate and safe method that allows the omission of physical medical guides regarding the surgical procedure. This most likely will reduce lead-time and thus reduce pressure on the planning. More time will be available to design an fabricate the obturator prosthesis, since this is the only medical device that needs to be brought to the operating theatre.

- 2. The data in this thesis is promising but is just phase I data. It is needed to both provide the long term data of this small cohort as well as to join with other centers to be able to perform multi center studies proving that indeed zygomatic implants placed at primary surgery with immediate loading with an obturator prosthesis is a favourable treatment option.
- 3. Multidisciplinary collaboration with radiotherapists during the preoperative virtual planning phase is needed to gain further insight into adapting radiation fields to implant reconstruction when feasible. A fully coordinated surgical, radiotherapeutic and prosthodontic plan is a future goal as this approach could greatly improve the quality of life for these patients.

Based on the studies in this thesis, the following conclusions can be drawn;

- Patients with maxillary cancer benefit from 3D workflows and this should be provided as standard care. In addition, it lowers the physical burden of patients due to a more efficient procedure and thereby reduces the necessary time for functional prosthodontic rehabilitation.
- Based on very promising treatment outcomes, guided placement of zygomatic implants for prosthodontic rehabilitation should be considered as a reliable rehabilitation treatment plan in case of large maxillary resections.
- Multidisciplinary collaboration should be further expanded, in particular aimed to incorporate radiotherapy planning prior to surgery. This approach can lead to significant improvement in rehabilitation outcomes and thus the quality of life for head and neck cancer patients.

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# **CHAPTER** APPENDICES

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#### **SUMMARY**

Treatment of tumours in the upper jaw requires multidisciplinary involvement due to their effects on oral functions, aesthetics, and psychological aspects. Choosing the appropriate rehabilitation for a maxillary defect depends on factors such as tumour characteristics, the size and position of the defect, the patient's health, and any associated conditions.

Prosthetic rehabilitation with an obturator prosthesis has historically been a good option for restoring defects in the upper jaw, but often suffers from insufficient retention. In case of insufficient bone in the upper jaw, zygomatic implants can be placed to improve retention of the obturator prosthesis in addition to using endosseus implants. However, an accurate placement of these long implants is challenging, and deviation from the desired implant position can negatively impact the quality and outcome of the prosthodontic rehabilitation.

Advanced digital planning techniques, such as three-dimensional virtual surgical planning (3D VSP), can help to improve the accuracy and predictability of surgical outcomes for head and neck oncology patients. The research compiled in this thesis contributes to the development and optimization of 3D workflows by combining the surgical planning of maxillary resections with complex prosthodontic rehabilitations in a 3D virtual surgical plan. This contributes to personalized and optimized prosthodontic care for head and neck cancer patients with a tumour in the upper jaw.

Early involvement of the maxillofacial prosthodontist (MFP) in the head and neck oncology care pathway ensures that the patient receives an early understanding of the prosthetic possibilities and the various treatments required. The importance of the MFP and the benefits of 3D technology for planning and prosthetic treatment are described in **Chapter 2.1.** It is expected that with the help of 3D technology, the prosthetic outcome and thus the quality of life of head and neck oncology patients can be improved.

One of the factors influencing the rehabilitation of head and neck oncology patients is the timing of implant placement. **Chapter 2.2** presents the outcome of a literature review on primary and secondary placement of implants. The primary outcome measure was 5-year implant survival. Sixteen studies were included. Based on the quantitative analysis, a higher 5-year implant survival rate was found for primary placed implants (92.8% (95% CI: 87.1%–98.5%)) compared to secondary placed implants (86.4% (95% CI: 77.0%–95.8%)). Not only because of the increased implant survival but also due to other advantages of primary implant placement (earlier prosthetic rehabilitation and, increased quality of life), it is advised to standardly combine resection surgery with implant placement in edentulous situation.

**Chapter 2.3** provides an overview of the latest developments of 3D VSP and computeraided design (CAD) for the (prosthetic) reconstruction of maxillary defects. 3D VSP allows preoperative planning of resection margins and osteotomies, and recent advancements in multimodal imaging and personalized implant development using CAD have improved the translation of 3D VSP into surgery. Additionally, techniques such as intraoperative imaging and augmented reality have improved the accuracy and precision of the procedure. With the use of 3D VSP and CAD, ablation surgery, reconstructive surgery and prosthetic rehabilitation can be planned preoperatively. The goal of maxillary defect rehabilitation is to restore facial form and oral function in accordance with the individual needs of the patient.

**Chapter 3** introduces a complete 3D workflow for immediate implant-fixed prosthetic rehabilitation after maxillary resection. This approach includes several steps, starting with 3D virtual surgical planning for tumour removal, followed by the placement of zygomatic implants and the fabrication of an obturator prosthesis that fits the planned situation and can be immediately fixed to the zygomatic implants. It is hypothesized that when specially designed guides are used, implants can be placed with such precision that they are suitable for immediate loading with an obturator prosthesis.

To test the feasibility of this approach, 3D virtual surgical planning was performed on five fresh frozen human cadavers for the resection of the maxilla and guided placement of ten zygomatic implants using custom cutting and drill/placement guides. A preoperatively designed and printed obturator prosthesis was placed and connected to the zygomatic implants. Accuracy of implant positioning was assessed by merging pre- and post-operative designed obturator prostheses matched the per-operative implant positions accurately, allowing for immediate loading. The mean prosthetic point deviation on the cadavers was  $1.03 \pm 0.85$  mm, the mean entry point deviation was 1.20  $\pm$  0.62 mm, and the 3D angular deviation was 2.97  $\pm$  1.44°. These results demonstrate the feasibility of 3D virtual surgical planning for accurate execution of ablative maxillary surgery, zygomatic implant placement, and placement of an immediate implant-retained obturator prosthesis. The next step is to apply this workflow in the operating room for patients undergoing maxillectomy.

**Chapter 4** evaluates the 3D VSP method for placing zygomatic implants from Chapter 3 in patients. In ten patients, partial maxillary resection was performed, followed by the placement of zygomatic implants using 3D VSP and 3D-printed patient-specific guides. The study aims to assess the accuracy of zygomatic implant placement and the fit of the obturator prostheses in this one-stage procedure. The results showed that zygomatic implants ( $n = 28$ ) were placed with good accuracy (mean deviation 1.73  $\pm$  0.57 mm and  $2.97 \pm 1.38$ ° 3D angular deviation. The 3D accuracy of the prosthetic platform position was  $1.58 \pm 1.66$  mm, with an accuracy of  $2.21 \pm 1.33$  mm in the occlusal plane, and a height accuracy of  $1.32 \pm 1.57$  mm. Additionally, in all cases the obturator prothesis fitted as pre- operatively planned. This feasibility study shows that this novel application of 3D-printed surgical drill guides results in predictable zygomatic implant placement and provides the possibility of immediate prosthetic rehabilitation in head and neck oncology patients after maxillectomy.

**Chapter 5** describes the immediate loading of guided placed zygomatic implants and its impact on implant survival rates after at least 12 months. The study shows good survival rates for zygomatic implants up to three years post-treatment. There was a trend of higher implant loss in irradiated patients (100% without radiation; 85% in irradiated patients). The study emphasized the importance of evaluating not only the success of implant placement and the fit of the obturator prosthesis but also the quality of life (QoL) of patients post-treatment. Patients reported favourable outcomes regarding QoL, although some reported issues with xerostomia and limited mouth opening, especially those who had undergone radiation therapy. The study highlighted that the radiation dose to the zygomatic bone significantly impacts implant survival rates, and the tumour's position and size directly affected the radiation doses to the zygomatic bone. Further research is necessary, and closer collaboration between surgical teams and radiotherapists during the virtual surgical planning phase of treatment and rehabilitation is crucial to improve the survival rates of zygomatic implants in patients undergoing postoperative radiotherapy.

An important development in the reconstruction of the upper jaw is the possibility of designing patient-specific implant (PSI) to retain prostheses. In **Chapter 6**, we demonstrate the use of an implant for the rehabilitation of large maxillary defects in cases where direct or delayed surgical reconstruction is not feasible. The benefits of an easily removable obturator prosthesis are emphasized, allowing for tissue inspection and cleaning of the oral cavity and defect by the patient.

3D techniques enable the creation of a patient-specific design, as demonstrated in this study. It provides a solution for patients when more conventional treatment options are not possible. The possibility of adequate prosthetic rehabilitation has a direct positive impact on oral functions and quality of life of the patient. We performed a finite element analysis (FEA) to ensure rigidity of the implant design. We achieved a maximum deviation of 0.44 mm compared to preoperative scans, indicating accurate placement. Despite the success reported in this case, several unanswered questions remain regarding optimal technical principles. It is anticipated that guidelines will be developed to support the design of patient-specific implants.

In the general discussion (**Chapter 7**), the results of the previous studies are further discussed. Based on the findings of the research, several recommendations and perspectives for future studies are given.

#### **SAMENVATTING**

Behandeling van tumoren in de bovenkaak vereisen een multidisciplinaire aanpak vanwege het effect op mondfuncties, esthetiek en psychologische aspecten. Het kiezen van de juiste rehabilitatie van een defect in de bovenkaak hangt af van meerdere factoren, zoals tumor eigenschappen, de grootte en positie van het defect, de gezondheid van de patiënt en eventuele bijkomende aandoeningen.

Prothetische rehabilitatie met een obturator prothese is historisch gezien een goede optie voor het herstellen van defecten in de bovenkaak, maar hebben als nadeel dat vaak de houvast van de prothese onvoldoende is. Naast het gebruik van klassieke implantaten kunnen, indien er te weinig bot is in de bovenkaak, zygoma implantaten worden geplaatst ter ondersteuning van de obturator prothese. Echter, het nauwkeurig plaatsen van deze lange implantaten is een uitdaging waarbij een afwijkende implantaat positie ten opzichte van de gewenste situatie een negatieve invloed kan hebben op de kwaliteit en uitkomst van de prothetische eindsituatie.

Geavanceerde digitale planningstechnieken zoals driedimensionale virtuele chirurgische planning (3D VSP) kunnen helpen bij het verbeteren van de nauwkeurigheid en het voorspelbaar maken van chirurgische uitkomsten bij hoofd-hals oncologie patiënten. Het onderzoek gebundeld in dit proefschrift draagt bij aan de ontwikkeling en het optimaliseren van 3D workflows, door het combineren van de chirurgische planning van bovenkaaksresecties met de complexe prothetische rehabilitaties in een 3D virtueel chirurgisch plan. Dit draagt bij aan gepersonaliseerde behandelkeuzes met optimalisatie van prothetische zorg voor patiënten met een tumor in de bovenkaak.

Vroege betrokkenheid van de tandarts maxillofaciale prothetiek (MFP) in het hoofd hals oncologie zorgpad zorgt ervoor dat de patiënt al tijdig in het behandeltraject een beeld krijgt van de prothetische (on)mogelijkheden en de diverse behandelingen die benodigd zijn. Het belang van de tandarts MFP en de voordelen van 3D technologie voor de planning en prothetische behandeling worden beschreven in **hoofdstuk 2.1**. De verwachting is dat met behulp van 3D technologie de prothetische uitkomsten en daarmee de kwaliteit van leven van hoofdhals oncologie patiënten kunnen verbeteren.

Eén van de factoren die van invloed is op de rehabilitatie van hoofd-hals oncologie patiënten is de timing van het plaatsen van implantaten. In **hoofdstuk 2.2** wordt de uitkomst van een literatuuroverzicht gepresenteerd over primair en secundair geplaatste implantaten beschreven. De primaire uitkomstmaat was 5-jaars implantaatoverleving. 16 studies werden geïncludeerd. Op basis van de kwantitatieve analyse werd een hogere 5-jaars implantaatoverleving gevonden voor primair geplaatste implantaten (92.8% (95% CI: 87.1%–98.5%)) dan voor secundair geplaatste implantaten (86.4% (95% CI: 77.0%–95.8%)). Niet alleen vanwege de verhoogde implantaatoverleving, maar ook vanwege de andere voordelen van primaire implantaat plaatsing (snellere prothetische rehabilitatie, toegenomen kwaliteit van leven) wordt geadviseerd om resectie chirurgie standaard te combineren met het plaatsen van implantaten in edentate kaken.

In **hoofdstuk 2.3** wordt een overzicht gegeven van recente ontwikkelingen van 3D VSP en computerondersteund ontwerp (CAD) voor de (prothetische) reconstructie van defecten in de bovenkaak. 3D VCP maakt preoperatieve planning van resectiemarges en zaagvlakken mogelijk. Recente ontwikkelingen in multimodale beeldvorming en gepersonaliseerde implantaat ontwikkeling met behulp van CAD hebben de vertaling van 3D VSP naar de chirurgie verbeterd. Bovendien hebben technieken zoals intraoperatieve beeldvorming en augmented reality de nauwkeurigheid en precisie van de procedure verbeterd. Het doel van reconstructie van de bovenkaak is om het profiel van het gelaat en mondfuncties zo goed mogelijk te herstellen, in overeenstemming met de individuele behoeften van de patiënt.

In **hoofdstuk 3** wordt een volledige 3D-workflow geïntroduceerd voor direct implantaat gefixeerde prothetische rehabilitatie na resectie van de bovenkaak. De aanpak omvat verschillende stappen, beginnend met 3D-virtuele chirurgische planning voor het verwijderen van tumoren, gevolgd door het plaatsen van zygoma-implantaten en het vervaardigen van een obturator prothese die past bij de geplande situatie en direct gefixeerd kan worden op de zygoma implantaten.

Om de haalbaarheid van deze aanpak te onderzoeken, werden de procedures uitgevoerd op vijf kadavers. Met behulp van op maat gemaakte zaag- en boormallen werd eerst de resectie van de maxilla uitgevoerd en vervolgens geleid de zygoma-implantaten geplaatst. Hierna werd een preoperatief ontworpen en geprinte obturator prothese geplaatst en verbonden met de geplaatste zygoma implantaten. Nauwkeurigheid was van cruciaal belang en om de positie van de implantaten te controleren werden 3D-afwijkinganalyse uitgevoerd door de pre- en postoperatieve CT-scans te combineren. De resultaten waren veelbelovend: de preoperatief ontworpen obturator protheses pasten nauwkeurig bij de peroperatieve implantaatposities en konden allen worden geplaatst en gefixeerd voor onmiddellijke belasting.

De gemiddelde afwijkingen waren minimaal: de afwijking van het prothetische punt bedroeg  $1,03 \pm 0,85$  mm, de afwijking van het ingangspunt was  $1,20 \pm 0,62$  mm, en de 3D-hoekafwijking was 2,97 ± 1,44°. Deze resultaten tonen aan dat het mogelijk is om met behulp van 3D VSP nauwkeurig de chirurgische resectie, implantatie van zygoma implantaten en een preoperatief vervaardigde obturator prothese direct te fixeren en het maxillaire defect goed af te sluiten. De volgende stap is het toepassen van deze workflow in de operatiekamer bij patiënten die een maxillectomie moeten ondergaan.

In **hoofdstuk 4** wordt de daadwerkelijke uitvoering van de 3D VCP methode omtrent de plaatsing van zygoma implantaten uit hoofdstuk 3 geëvalueerd bij patiënten. Bij tien patiënten is er een gedeeltelijke resectie van de bovenkaak uitgevoerd en werden vervolgens zygoma implantaten geplaatst met behulp van 3D VSP en 3D geprinte patiënt specifieke mallen. Het doel van de studie is om de nauwkeurigheid van de plaatsing van de zygoma implantaten en de pasvorm van de obturator protheses bij deze een fase procedure te beoordelen. Zygoma implantaten (n = 28) werden geplaatst met goede nauwkeurigheid (gemiddelde afwijking 1,73 ± 0,57 mm en 2,97 ± 1,38° 3D-hoekafwijking) en in alle gevallen paste de obturator prothese zoals vooraf gepland. De 3D-nauwkeurigheid van de positie van het prothetisch platform was 1,58 ± 1,66 mm, waarbij de nauwkeurigheid ter hoogte van het occlusale vlak 2,21 ± 1,33 mm was , met een hoogte nauwkeurigheid van 1,32 ± 1,57 mm. Deze haalbaarheidsstudie toont aan dat de toepassing van deze nieuw ontworpen 3D-geprinte chirurgische boormallen resulteert in voorspelbare plaatsing van zygoma implantaten en de mogelijkheid biedt van directe prothetische rehabilitatie bij patiënten die een bovenkaaksresectie moeten ondergaan.

De directe belasting van op geleide geplaatste zygoma implantaten en de impact ervan op het overlevingspercentage van implantaten na minimaal 12 maanden wordt in **hoofdstuk 5** beschreven. De studie laat gunstige overlevingspercentages zien van de zygoma implantaten tot drie jaar na de behandeling, maar er was een trend van meer implantaatverlies bij bestraalde patiënten (100% zonder bestraling; 85% bij bestraalde patiënten). De studie benadrukt het belang van het evalueren van niet alleen het succes van de implantaat plaatsing en de obturator prothese, maar ook van de kwaliteit van leven (QoL) van patiënten na behandeling. Patiënten meldden gunstige resultaten wat betreft hun QoL, hoewel sommigen problemen meldden betreffende xerostomie en een beperkte mondopening, vooral degenen die bestralingstherapie hadden ondergaan. De studie benadrukte dat de bestralingsdosis op het zygoma bot een significante invloed heeft op de overlevingspercentages van implantaten. De positie en grootte van de tumor beïnvloedden rechtstreeks die bestralingsdoses op het zygoma bot. De noodzaak van verder onderzoek werd benadrukt en een nauwere samenwerking tussen chirurgische teams en radiotherapeuten in de planningsfase van behandeling en rehabilitatie wordt cruciaal geacht om de overlevingspercentages van ZI te verbeteren bij patiënten die postoperatieve radiotherapie ondergaan.

Een belangrijke ontwikkeling in de reconstructie van de bovenkaak is de mogelijkheid van het patiënt specifiek ontwerpen van implantaten (PSI's) voor verbetering van het houvast voor obturator protheses. In **hoofdstuk 6** demonstreren we het gebruik van een implantaat voor de rehabilitatie van grote maxillaire defecten in gevallen waarin directe of uitgestelde chirurgische reconstructie niet haalbaar is. De voordelen van een gemakkelijk verwijderbare obturator prothese worden benadrukt, waardoor weefselonderzoek en reiniging van de mondholte en defect door de patiënt mogelijk zijn.

3D technieken maken het mogelijk om een patiënt specifiek ontwerp te maken zoals is aangetoond in deze studie. Het biedt een oplossing voor patiënten als de meer reguliere behandelopties niet mogelijk zijn. De mogelijkheid tot een adequate prothetische rehabilitatie heeft direct een positieve invloed op de mondfuncties en kwaliteit van leven. Er werd een eindig-elementanalyse (FEA) uitgevoerd om de sterkte van het implantaatontwerp te waarborgen. We bereikten een maximale afwijking van 0,44 mm in vergelijking met preoperatieve scans, wat wijst op nauwkeurige plaatsing. Ondanks het succes dat in dit geval wordt gemeld, blijven er verschillende onbeantwoorde vragen bestaan over optimale technische principes. Het is te verwachten dat richtlijnen zullen worden ontwikkeld ter ondersteuning voor het ontwerpen van patiënt specifieke implantaten.

In de algemene discussie (**hoofdstuk 7**) worden de resultaten van voorgaande studies verder bediscussieerd. Op basis van de bevindingen uit de onderzoeken worden enkele aanbevelingen en perspectieven voor toekomstige studies gegeven.

## **DANKWOORD**

Ik had nooit gedacht dat ik, na 12 jaar werken als tandarts in mijn eigen praktijk, nog zou starten met de opleiding tot tandarts Maxillofaciale Prothetiek (MFP) in Groningen. Het bleek een uitstekende keuze. De kans om na mijn opleiding als staflid te blijven bij de afdeling Mondziekten, Kaak- en Aangezichtschirurgie in het UMCG en te promoveren greep ik met beide handen aan. Ik vond het belangrijk om onderzoek te doen gerelateerd aan de behandeling van hoofd-hals oncologie patiënten. De patiëntengroep waar ik me samen met de collega's dagelijks voor inzet binnen het Centrum voor Bijzondere Tandheelkunde (CBT). Het boek dat nu voor u ligt is het resultaat. Dat de nieuwe behandelmogelijkheden die in dit onderzoek zijn beschreven inmiddels als reguliere zorg worden toegepast, zowel op onze afdeling als in andere hoofd-hals oncologie centra geeft een gevoel van trots. Zonder de bijdrage van velen was het niet mogelijk geweest dit proefschrift te maken. Daarom wil ik iedereen bedanken die, direct of indirect, hieraan heeft bijgedragen. Een aantal mensen wil ik in het bijzonder bedanken.

Allereerst gaat mijn dank uit naar de patiënten die betrokken waren bij de onderzoeken in dit proefschrift. Op een moeilijk moment in hun leven toonden ze hun vertrouwen en bereidwilligheid om mee te werken aan innovatieve behandelmethoden. Ik heb veel respect voor hun doorzettingsvermogen.

Prof. Dr. M.J.H. Witjes, hooggeleerde promotor, beste Max, dank voor je steun en begeleiding tijdens mijn promotieonderzoek. Je enthousiasme voor onderzoek is aanstekelijk en heeft mij geïnspireerd. Een paar maanden na de start van mijn opleiding tot tandarts MFP stond ik samen met jou op het operatiecentrum voor een complexe bovenkaaksresectie. De reconstructie was geheel 3D gepland en de prothese lag klaar om direct te worden geplaatst. De behandeling, samenwerking met andere specialisten en hoe jij oog had voor de prothetische fase van de behandeling, vond ik fantastisch. Je visie, "plan your operation and operate your plan" kwam daar voor mij tot leven. Dat ik nu onder jouw begeleiding onderzoek kon doen gericht op prothetische rehabilitatie van bovenkaaksresecties heeft zo moeten zijn. Dank voor het vertrouwen en de ruimte die je hebt gegeven om de digitalisering van de prothetische reconstructies mogelijk te maken. Ik kijk uit naar de aankomende jaren van samenwerken in patiëntenzorg en onderzoek.

Prof. Dr. G.M. Raghoebar, hooggeleerde promotor, beste Gerry, jij daagt me uit op een positieve manier en haalt het beste in mij naar boven. De discussies die we af en toe hebben, waar we stiekem beide van genieten, houden mij scherp en maken de behandelplannen beter. Implantologie en prothetiek zijn onlosmakelijk met elkaar verbonden en jouw kennis van de prothetische tandheelkunde maakt je uniek als kaakchirurg. Je was onmisbaar in het onderzoek met zygoma implantaten. Het is een voorrecht om met je te werken en samen de complexe zorg uit te voeren die voortkwam uit dit onderzoek. Je bent een briljant kaakchirurg-implantoloog maar vooral een mooi mens die aandacht heeft voor de mensen om zich heen. Je was er altijd op de momenten dat ik het echt nodig had. Dank voor je steun tijdens dit onderzoek maar ook voor je interesse in mij als persoon.

Dr. J. Kraeima, zeergeleerde promotor, beste Joep, jouw inbreng in dit onderzoek was ontzettend belangrijk. Samen hebben we de eerste digitale klosprothese designs uitgedacht vanuit tumorintekeningen en de zygoma implanaten gepland. Uiteindelijk heeft dit geleid tot een werkwijze die nu wordt overgenomen in diverse centra in het land. Jij zoekt altijd naar verbetermogelijkheden en een beetje snelheid houden we beide van! Op de weg heb ik liever 4 wielen. Ik rij graag nog eens samen met je naar een congres.

Dr. S.A.H.J. de Visscher, zeergeleerde copromotor, beste Sebastiaan, dit onderzoek heeft mede door jou vleugels gekregen. Vanaf de trip naar Londen en Keele om meer inzicht te krijgen in het gebruik van zygoma implantaten was je aan boord. Dank voor de bijdrage die je hebt geleverd aan het tot stand komen van dit proefschrift, je kritische noten bij de manuscripten waren zeer welkom. Ik hoop dat we nog vele jaren kunnen samenwerken.

Geachte Prof. Dr. H.J.A. Meijer, Prof. Dr. A.J.W.P. Rosenberg en Dr. G.B. Halmos, hartelijk dank voor uw bereidheid om in de leescommissie plaats te nemen en voor uw deskundige beoordeling van dit proefschrift.

Geachte Prof. Dr. F.K.L. Spijkervet, beste Fred, als afdelingshoofd maak je het CBT als onderdeel van de afdeling Mondziekten, Kaak-en Aangezichtschirurgie UMCG belangrijk. Je stimuleert hiermee de samenwerking tussen de kaakchirurgen en CBT tandartsen in de hoog complexe zorg en de bijbehorende onderzoekstrajecten. Persoonlijk wil ik je bedanken voor het vertrouwen in mij als hoofd CBT en voor de mogelijkheid om mijn promotieonderzoek op onze afdeling te kunnen doen.

Geachte medeleden van het Dagelijks Bestuur van de afdeling Mondziekten, Kaak- en Aangezichtschirurgie UMCG, beste Fred, Baucke, Ron, Judith en Angelika, dank voor de mogelijkheid om dit onderzoek te voltooien. Ik kijk uit naar onze verdere samenwerking.

Dr. H. Reintsema, beste Harry, Ik kan je niet genoeg bedanken voor de kans die je me hebt gegeven om de tandarts MFP te worden die ik vandaag de dag ben. Jij geeft me de ruimte om mijzelf te ontwikkelen maar staat altijd klaar als hulp nodig is. Ook bij dit onderzoek was je mijn vangnet. Jouw kennis van de prothetische rehabilitaties van hoofd-hals oncologie patiënten is ongekend en daar heb ik dankbaar gebruik van gemaakt. We hebben beide een nuchtere kijk op het leven en delen een passie voor de prothetische zorg. Vorig jaar heb ik jouw taken als hoofd CBT overgenomen en langzaam moeten we gaan wennen aan het idee dat jij over een paar maanden met pensioen gaat. Het lukt me nog niet om de afdeling voor te stellen zonder jou, maar gelukkig blijf je betrokken bij de opleiding MFP en kunnen we nog vele congressen samen bezoeken.

Dr. C. Stellingsma en mevr. M. Beenakker, beste Kees en Marije, fantastische collega's maar ook voor enkele jaren ontzettend lieve (bijna) buren. Door jullie voelde ik me nooit alleen in mijn studio aan de Petrus Campersingel. Jullie deur stond altijd open. Jullie hebben Danny en mij geholpen als starters in Groningen, door jullie voelden we ons welkom.

Dr. A. Korfage, Dr. W. Noorda, Prof. Dr. A. Visser en Prof. H.J.A. Meijer, beste Anke, Willem, Anita en Henny, samen met Harry en Kees waren jullie de stafleden van het CBT die mij een vliegende start hebben gegeven. Wat fijn dat jullie het vertrouwen hadden in mij. Dat was niet direct duidelijk na mijn sollicitatiegesprek maar inmiddels kunnen we daar hartelijk om lachen. Een tandarts uit Haarlem, in opleiding in Groningen, hoe dan? Het geeft aan hoe jullie niet denken in beperkingen maar in mogelijkheden (of er zijn echt geen tandartsen te krijgen in het Noorden en jullie dachten we zien wel). Welke versie het ook is, ik ben blij dat ik inmiddels full time als tandarts MFP in het UMCG werk. Door jullie heb ik mijn promotie onderzoek kunnen uitvoeren. Samen met de collega's in opleiding, Iris, Annelot, Emmanuelle en Gerry gaven jullie mij de tijd en ruimte en deden jullie zelf een stap harder in de patiëntenzorg. Dat is pas een team!

Ashwin Beekes en Maarten Heuvels, door jullie hulp is het gelukt de workflow voor klosprotheses te digitaliseren. Het vergt af en toe toch nog wel wat ouderwets analoog hard werken. Dank voor jullie enthousiasme en de fijne samenwerking.

Stafleden van de afdeling Mondziekten, Kaak- en Aangezichtschirurgie UMCG, dank voor jullie steun tijdens mijn promotieonderzoek. Jullie waren altijd bereid om te helpen.

Dr. J.M. Alberga, beste Jamie, onze promotietrajecten liepen deels gelijk op. We waren beide al stafleden en deden beide onderzoek binnen de hoofd-hals oncologie patiëntengroep. Dank voor je steun. We wisten elkaar te vinden als we even vastliepen en frustraties die altijd gepaard gaan bij onderzoek doen konden we bij elkaar kwijt. Ik kijk uit naar onze verdere samenwerking. Dank dat je mijn paranimf wil zijn.

Mondhygiënisten van de afdeling Mondziekten, Kaak- en Aangezichtschirurgie UMCG, Barbara van Eijkelenborg, Sanne Scholten, Wendy van der Goot-Roggen en Sitske Oort (jij hoort er voor mij ook gewoon nog bij!), jullie zijn onmisbaar in de patiëntenzorg van het CBT. Jullie rol in het hoofd-hals oncologie zorgpad is ontzettend belangrijk en door jullie hulp liep de inclusie van de patiënten voor mijn onderzoek als een trein. Ik hoop nog heel lang met jullie samen te werken en de spreekuren van Crazy Friday en inmiddels ook Crazy Thursday, samen vol goede moed en een gezonde dosis humor tot een goed einde te brengen.

Dr. ing. B.J. Merema, beste Bram, je design skills zijn onmisbaar geweest voor mijn onderzoek. Om de ideeën om te zetten in beelden op het scherm vergt inzet en tijd, mijn dank hiervoor.

Beste collega's van het 3D lab, tussen de patiëntenzorg door even langs om planningen en guides te beoordelen terwijl jullie het zelf ook smoordruk hebben. Het kan en mag altijd. Dank voor jullie flexibiliteit en hulp bij mijn onderzoek. Het eerstvolgende rondje bij een van de gezellige 3D uitjes is van mij!

Mathilda Massier, aan jou mijn persoonlijke dank. Sinds de dag dat ik in opleiding kwam hebben we veel samengewerkt. Jouw hulp bij de complexe behandelingen die voortkwamen uit mijn onderzoek betekent veel voor mij. Samen met Annet, Ingrid en Tanja werden nieuwe prothetische onderdelen en implantaten altijd op tijd besteld. Voor jullie engelengeduld met het meest onpraktische bestelsysteem ever, ERP, heb ik veel bewondering.

Beste collega's van de medische administratie afdeling Mondziekten, Kaak- en Aangezichtschirurgie UMCG, in het bijzonder Loura van der Veen, Henriët Spanjer, Inge Miske-van der Boor en Renate Hartman-Kolhek, dank voor jullie hulp ook tijdens dit onderzoek. Jullie hebben wonderen verricht met het plannen van de onderzoekspatiënten.

Beste dames van de röntgen, alle onderzoekspatiënten inclusief losse protheses met scanmarkers hebben jullie prachtig gescand, waarvoor dank. Het uitgedachte scan protocol t.b.v. planning van zygoma implantaten werkt fantastisch. Dank voor de perfecte plaatjes!

Alle overige collega's van de afdeling Mondziekten, Kaak- en Aangezichtschirurgie; AIOS, assistentie, collega's van de sterilisatie, onderzoekers. Jullie zijn fantastisch. Dank voor de goede samenwerking. Jullie hulp en interesse in mijn onderzoek is hartverwarmend.

Beste Angelika, Lisa, Nienke en Fieke, dames van het secretariaat Mondziekten, Kaak- en Aangezichtschirurgie UMCG. Bedankt voor jullie hulp en ondersteuning. Lisa, jij was voor mij van onschatbare waarde tijdens dit promotieonderzoek. Bij vragen over onderzoek heb je niet alleen een antwoord maar hulp wordt ook direct geboden. Je bent het geheime wapen van vele onderzoekers.

Beste (oud) collega's uit het Medisch Centrum Leeuwarden. Bij jullie is het allemaal begonnen! Dank dat jullie mij met open armen hebben ontvangen en mijn start in de bijzondere tandheelkunde hebben mogelijk gemaakt. Ik kijk met veel plezier terug op de jaren in het MCL.

Drs. L Brummelkamp, lieve Liselot, wat hebben we veel meegemaakt samen. Lief en leed gedeeld tijdens de studie Tandheelkunde en gedurende onze praktijkjaren aan de Wilhelminastraat en later de Sophiastraat. Als vriendinnen en jonge ondernemers met een gezonde dosis lef hebben we ons vrij gevestigd in centrum Haarlem. Verbouwen deden we zelf. Het maken van complexe planningen, 3D inzicht hebben we toen al geleerd. Het waren prachtige jaren en ik had dit met niemand anders kunnen en willen beleven. We hebben aan een woord genoeg en vullen elkaar als tandartsen en zakenpartners perfect aan. Nog altijd ben ik trots op de praktijk die we hebben opgebouwd en ik ben benieuwd naar de mooie ontwikkelingen die jij voor ogen hebt met de praktijk die nu toch echt helemaal van jou is. Ik heb heel veel van je geleerd en het was een moeilijke tijd toen ik mijn hart volgde en koos voor de bijzondere tandheelkunde en het UMCG. Dank voor je steun en de ruimte die je me hebt gegeven om mijn doelen te bereiken. Ik hoop dat jouw dromen ook uitkomen.

Assistentes en mondhygiënisten Tandartspraktijk Brummelkamp & Vosselman, jullie zijn de beste. Dank voor alle mooie jaren van samenwerking. Uit het oog maar zeker niet uit het hart.

Lieve meiden, Angeles, Diana en Miranda, al bijna 40 jaar zijn we een mooi stel samen. Vriendinnen voor het leven, dat was al bepaald in de eerste klas van de basisschool. Jullie zijn er altijd, of ik het nu wil of niet. Het leven is zoveel leuker met jullie. Dank voor jullie steun, de ontelbare etentjes, gevraagde en ongevraagde meningen en onvoorwaardelijke vriendschap. Angeles, dank dat je mijn paranimf wil zijn.

Lieve mama, dank je wel voor jouw onvoorwaardelijke steun en liefde. Je kracht en positiviteit zijn ongekend en een voorbeeld voor mij en velen om ons heen. We hebben moeilijke tijden gekend, van jongs af aan heb je me geleerd om te genieten van het leven ondanks tegenslagen en te kiezen voor wat je echt gelukkig maakt. Mijn keuze om dat geluk in Groningen na te streven was moeilijk voor je, zo ver weg. Maar gelukkig zit Rotterdam in mijn DNA en een trip naar 010, om even een rondje door de stad te maken en bij je langs te gaan, zijn voor ons beide mooie momenten. Wat fijn dat je er bij bent op mijn promotie.

Broer en zus, Patrick en Chantal, het leven gaat niet altijd over rozen. Ik ben trots op wat we hebben bereikt. We zijn ontzettend verschillend maar doorzettingsvermogen hebben we alle drie gemeen. Ik hou van jullie.

Lieve Danny, zonder jou was dit proefschrift er niet gekomen. Dank voor het brengen van rust en humor op de momenten dat dit nodig was en dat mijn werk en onderzoek af en toe voor mogen gaan. Jij brengt evenwicht in mijn leven en samen hebben we de mooiste plannen werkelijk gemaakt. Het roer om, verhuizen naar Groningen, voor jou een nieuwe baan omdat ik zo graag in het UMCG wil werken, dit samen met een ongewone collectie huisdieren, (bijna) niets is te gek, je bent fantastisch. Ik hou van je.

# **ABOUT THE AUTHOR**

Nathalie Vosselman was born on 7th of Januari,1979, in Rotterdam, The Netherlands. After finishing secondary school in 1998 she studied dentistry at the University of Amsterdam and graduated in 2003. She started her private dental practice in Haarlem were she mainly provided complex restorative and prosthetic dental care for 17 years. Following completion of her training in Maxillofacial Prosthodontics in 2018 Nathalie works as fulltime staffmember at the department of Oral and Maxillofacial Surgery in the UMCG. As maxillofacial prosthodontist of the Head and Neck Oncology Centre she primarily focuses on oral and facial rehabilitation, in particular 3D workflows in prosthodontic rehabilitation of Head and Neck cancer patients. In 2023 Nathalie was appointed Head of the Centre for Special Dental Care at the Department of Oral and Maxillofacial Surgery, University Medical Center Groningen (UMCG). In this capacity, she oversees a team dedicated to providing specialized dental care to patients with complex needs.

Nathalie lives together with Danny Beenen and they joyfully share their home with multiple pets, in the serene countryside of Engelbert, Groningen.

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